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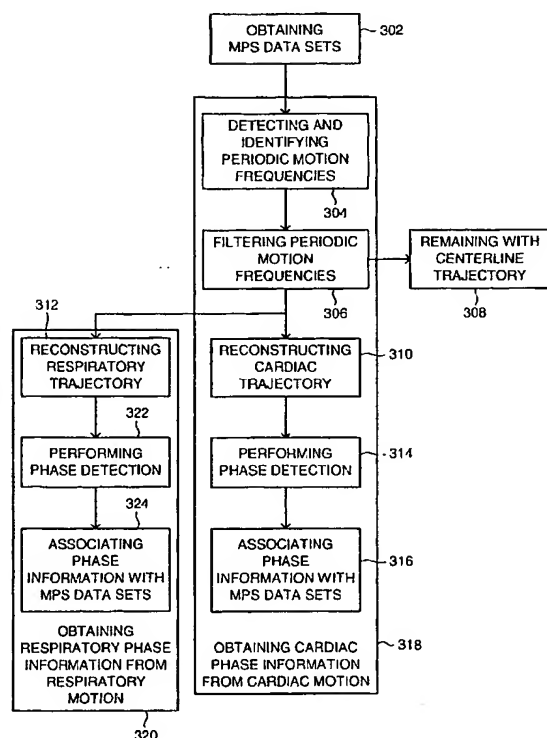
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(54) Title: METHOD AND APPARATUS FOR INVASIVE DEVICE TRACKING USING ORGAN TIMING SIGNAL GENERATED FROM MPS SENSORS



(57) Abstract: Apparatus for generating an organ timing signal relating to an inspected organ within the body of a patient, including a medical positioning system, and a processor coupled with the medical positioning system, the medical positioning system including at least one reference electromagnetic transducer placed at a reference location, at least one inner electromagnetic transducer attached to a surgical tool inserted in a blood vessel in the vicinity of the inspected organ, and a medical positioning system processor coupled with the reference electromagnetic transducer and the inner electromagnetic transducer, the medical positioning system processor determining the three-dimensional position of the inner electromagnetic transducer, by processing transmitted electromagnetic signals transmitted from one of the reference electromagnetic transducer and the inner electromagnetic transducer with detected electromagnetic signals detected by the other of the reference electromagnetic transducer and the inner electromagnetic transducer, the medical positioning system processor further generating medical positioning system data sets, each of the medical positioning system data sets including a collection of three-dimensional position coordinate readings demonstrating the motion trajectory of the surgical tool over time, the processor generating the organ timing signal from the medical positioning system data sets by detecting and identifying periodic motion frequencies in the medical positioning system data sets, and filtering the periodic motion frequencies from the medical positioning system data sets.



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METHOD AND APPARATUS FOR INVASIVE DEVICE TRACKING USING ORGAN TIMING SIGNAL GENERATED FROM MPS SENSORS

FIELD OF THE DISCLOSED TECHNIQUE

5 The disclosed technique relates to medical diagnostics and surgery systems and methods in general, and to a method and system for monitoring organ phases in three-dimensional medical imaging and navigation, in particular.

BACKGROUND OF THE DISCLOSED TECHNIQUE

10 Medical imaging is a powerful tool to assist in the performance of various types of medical operations, and to enhance diagnostics and other decisions concerning a medical procedure. Several systems are known in the art to produce real-time medical images via a variety of different
15 imaging modalities. In instances of imaging of anatomical structures that involve periodic motion or cyclic phases, the imaging system may encompass a timing element to take this into account. Monitoring devices, such as an electrocardiogram (ECG) machine, are regularly incorporated into medical imaging systems to provide timing information for registering
20 the captured images with respect to organ phase. Typically, the timing information obtained from such monitoring devices is not completely accurate. As well, the signal received from such monitoring devices involves a delay, and is not obtained in real-time with respect to the actual organ motion. Finally, an external monitoring device adds a cumbersome
25 element to an already complex system.

 US Patent 5,577,502 to Darrow et al entitled "Imaging of interventional devices during medical procedures", is directed to a method for compensation of subject motion during tracking of an invasive device within the body of the subject. A device tracking unit determines the
30 location of the invasive device relative to a fixed reference point. An

imaging device acquires a reference image of the subject. A position detection means placed within the imaging device measures the location over time of a reference point of the subject. Each acquired image is stored together with the corresponding location of subject reference point.

5 A subject tracking unit receives location information over time from position detection means, and computes translation and rotation movement of the subject from time of image acquisition to time of device location measurement. A registration unit receives the reference image, the net position and orientation change of the subject, and the device
10 location. The registration unit translates and rotates the reference image to match the position and orientation of subject at the time of device location measurement. An image of the device is superimposed upon the translated/rotated image of the subject at its absolute position and orientation. The registration unit may also adjust the displayed location of
15 the device, rather than the display of the image.

In addition to translation and rotation motion, the registration unit accounts for expansion and contraction of the subject, occurring due to a periodic motion cycle, such as the respiratory or cardiac cycles. Position detection means measures the change in the subject due to expansion
20 and contraction, and feeds this information to the registration unit. The registration unit distorts the reference image in accordance with the expansion and contraction, and subsequent translation and rotation, thereby dynamically registering the image of the subject with the current device location.

25 Alternatively, the imaging device may monitor subject motion by obtaining subsequent projections of the subject and then detecting offset and cross-sectional size of the subject in these images. Further alternatively, a series of reference images are each gated to the periodic motion cycle. The imaging device acquires a series of images at different
30 times within the cardiac cycle, as measured by an ECG signal. An ECG provides a signal for each measurement of device location. At a given

time, an image from the series which corresponds to the ECG signal is selected as the reference image. The registration unit translates and rotates this reference image, with respect to the information received from the subject tracking unit for that time. A representation of the measured
5 location of the device is superimposed upon the updated image, resulting in a registered image of the subject and the invasive device.

US Patent 5,622,174 to Yamazaki entitled "Ultrasonic diagnostic apparatus and image displaying system", is directed to a system for determining movement velocities of a moving internal organ and providing
10 a color display of the movement velocities over time. An ultrasonic probe transmits an ultrasound beam toward the heart. The transmitted ultrasonic beam is partially reflected by tissues of the heart as an echo signal and returned to the probe. The echo signal has a Doppler shift in frequency due to the Doppler effect. The echo signal is transduced into a voltage
15 signal and supplied to a reception signal processor. The signal is beam-formed, detected and output to a B-mode digital scan converter (DSC). The B-mode DSC converts the image data of the signal to standard television scanning data, which is sent to an image synthesizer. The B-mode DSC also stores a plurality of image data at arbitrary cardiac timing
20 in a B-mode frame memory.

The reception signal processor also sends the transduced echo signal to a phase detector. The phase detector performs phase detection on the Doppler shift frequency to extract the Doppler shift signal. A low pass filter filters out unnecessary Doppler signals resulting from valve
25 motion or blood flow, leaving only the Doppler signal from the cardiac muscle. A frequency analyzer calculates physical values relating to the velocities at each sampling volume of a scan plane, using the Fast Fourier Transform (FFT) or auto-correlation method. These values include mean Doppler frequencies (corresponding to mean velocities of movement of the
30 organ), variance (turbulence factors of Doppler spectrum), and maximum values of Doppler shift frequencies (maximum velocities of organ

movement at sampling volume). These values are sent as color Doppler information to a vector-velocity calculator, which calculates the absolute movement velocities of the organ at each sampling volume point. A display presents the magnitude and/or direction of velocities, in accordance with a color scheme assignment. It is noted that detected ECG signals of the heart are used to trigger the signal generator (output reference pulses for transmission/reception of ultrasonic beams). In addition, these cardiac timing signals are used to produce a real-time image displaying changes in movement velocities of the heart in color.

US Patent 6,246,898 to Vesely et al entitled "Method for carrying out a medical procedure using a three-dimensional imaging and tracking system", is directed to a method for performing an in-vivo medical procedure on an associated body using three-dimensional tracking and imaging. A plurality of transceivers is used to track the three-dimensional motion of an object under investigation. At least four transceivers are implanted within a specimen in whom distances are to be measured. Three transceivers lie in a (x,y) plane and act as a reference. The fourth transceiver determines the z-coordinates of surrounding transducers by determining if an active one of the transducers lies above or below the reference plane established by the three transceivers. Each of a plurality of transmitters attached to the specimen at various locations is sequentially fired, while the three reference transceivers record the receiver signals. Since the difference from each transmitter to the reference plane is known, the relative x,y,z coordinates of the transmitters can be determined using triangulation.

The video display is synchronized with the real-time patient heart beat using an ECG signal. An Analog-to-Digital (A/D) converter converts the ECG signal into digital data. A sync generator module produces a timing signal corresponding to the current heart activity from the digital ECG data. This is done by activating a memory location or input port, or generating an interrupt, at the precise time a QRS complex is identified. In

particular, the sync generator module tests the data signal for large rates of change, zero crossings, and other information allowing the sync generator module to reveal the QRS complex of the signal

US Patent Application 6,556,695 to Packer et al entitled "Method
5 for producing high resolution real-time images, of structure and function during medical procedures", is directed to a method for providing medical images in real-time to assist physicians in the performance of medical procedures. A Medical Resonance Imaging (MRI) system obtains a high resolution model of the heart prior to the medical procedure. Images of the
10 heart are acquired during successive cardiac phases. A pulse generator creates a series of fast gradient echo pulse sequences. The R-R interval of the cardiac cycle is divided up into several short segments of pulse sequences, using an ECG gating signal that triggers at the peak of the R wave. A single coordinate, or view, of the heart is acquired during each
15 fast gradient echo segment. Adjacent segments are combined into groups, and the data in each group contributes to generating an image at a different phase of the cardiac cycle. A number (e.g., fifteen) of two-dimensional slices are acquired during an entire cardiac cycle, depicting one slice through the heart at (e.g., fifteen) successive phases of the
20 cardiac cycle. Additional slices of the heart are acquired and reconstructed into two-dimensional images. These two-dimensional slices are then combined to form (e.g., fifteen) three-dimensional image data sets.

During the medical procedure, an ultrasonic transducer acquires low-resolution image frames of the heart in real-time. An ECG signal from
25 the patient detects the real-time cardiac phase. The stored high-resolution heart model is registered using the real-time image frames and ECG signal. The registered high-resolution model is then used to produce high-resolution, large field of view images in real-time on a display.

SUMMARY OF THE DISCLOSED TECHNIQUE

It is an object of the disclosed technique to provide a novel method and apparatus for intra-body navigation and invasive device tracking using an organ timing signal, which is generated without an external monitoring device.

In accordance with the disclosed technique, there is thus provided an apparatus for generating an organ timing signal relating to at least one inspected organ within the body of a patient. The apparatus includes a medical positioning system (MPS) and a processor. The processor is coupled with the MPS. The MPS includes at least one reference electromagnetic transducer, at least one inner electromagnetic transducer, and an MPS processor. The MPS processor is coupled with the reference electromagnetic transducer and with the inner electromagnetic transducer. The inner electromagnetic transducer is attached to a surgical tool inserted in a blood vessel in the vicinity of the inspected organ. The MPS processor determines the three-dimensional position of the inner electromagnetic transducer, by processing transmitted electromagnetic signals transmitted from one of the reference electromagnetic transducer and the inner electromagnetic transducer with detected electromagnetic signals detected by the other of the reference electromagnetic transducer and the inner electromagnetic transducer. The MPS processor further generates MPS data sets. Each of the MPS data sets includes a collection of three-dimensional position coordinate readings demonstrating the motion trajectory of the surgical tool over time. The processor generates the organ timing signal from the MPS data sets by detecting and identifying periodic motion frequencies in the MPS data sets, and filtering the periodic motion frequencies from the MPS data sets.

According to the disclosed technique, there is also provided a method for generating an organ timing signal relating to an inspected organ within the body of a patient. The method includes the procedures of

transmitting electromagnetic signals and detecting the electromagnetic signals, processing the transmitted electromagnetic signals with the detected electromagnetic signals, and determining the three-dimensional position of a surgical tool inserted within the body of a patient based on the

5 processing. The method further includes the procedures of generating MPS data sets comprising a collection of three-dimensional position coordinate readings demonstrating the motion trajectory of the surgical tool over time, detecting and identifying periodic motion frequencies in the MPS data sets, and filtering the periodic motion frequencies from the MPS

10 data sets.

BRIEF DESCRIPTION OF THE DRAWINGS

The disclosed technique will be understood and appreciated more fully from the following detailed description taken in conjunction with
5 the drawings in which:

Figure 1 is a schematic illustration of a system, constructed and operative in accordance with an embodiment of the disclosed technique;

Figure 2 is a block diagram of a method for registering three-dimensional magnetic coordinates into two-dimensional optical
10 coordinates, operative in accordance with another embodiment of the disclosed technique;

Figure 3 is a block diagram of a method for obtaining phase information from MPS data sets, operative in accordance with a further embodiment of the disclosed technique;

15 Figure 4A is a schematic illustration of a sample cardiac trajectory, in electrical signal representation and in mechanical signal representation;

Figure 4B is a schematic illustration of a sample respiratory trajectory in mechanical signal representation;

20 Figure 5 is a schematic illustration of a trajectory of the surgical tool of the system of Figure 1, inside a vessel in the body of a patient, respective of different activity-states of the cardiac trajectory of Figure 4;

Figure 6 is a schematic illustration of trajectories of a guided surgical tool inside a vessel in the body of a patient, each trajectory
25 processed with respect to a different activity-state;

Figure 7 is a block diagram of a method for superimposing MPS data onto two-dimensional image data for corresponding data sets, operative in accordance with another embodiment of the disclosed technique;

30 Figure 8 is a block diagram of a method for superimposing MPS data onto two-dimensional image data for non-corresponding data sets,

operative in accordance with a further embodiment of the disclosed technique;

Figure 9 is a block diagram of a method for constructing trajectories of a guided surgical tool within the body of a patient, respective
5 of different activity-states of an inspected organ, operative in accordance with another embodiment of the disclosed technique; and

Figure 10 is a block diagram of an additional method for constructing trajectories of a guided surgical tool within the body of a patient, respective of different activity-states of an inspected organ,
10 operative in accordance with a further embodiment of the disclosed technique.

DETAILED DESCRIPTION OF THE EMBODIMENTS

The disclosed technique overcomes the disadvantages of the prior art by providing methods and apparatus for intra-body navigation and
5 invasive device tracking using an organ timing signal generated without an external monitoring device. It is noted that the terms "phase" and "activity-state" are used interchangeably herein below. According to one embodiment, phase information is generated from a sensor which concurrently provides position and orientation information. The system
10 allows for image acquisition and playback, three-dimensional model reconstruction, intra-body navigation, and tracking an invasive device during minimally invasive surgery. These aspects are further explained in US Patent Application 2002/0049375 to Strommer et al entitled "Method and apparatus for real time quantitative three-dimensional image
15 reconstruction of a moving organ and intra-body navigation", which is hereby incorporated by reference. Also, the system can be used to optimally advise on the type and dimensions of surgical tool to insert, where the surgical tool should be inserted, and other decisions related to a surgical procedure.

20 Reference is now made to Figure 1, which is a schematic illustration of a system, generally referenced 100, constructed and operative in accordance with an embodiment of the disclosed technique.

System 100 includes a Medical Positioning System (MPS) 102, a medical imaging device 104, a database 106, a processor 108, a display
25 110, an image detector 116, a plurality of MPS sensors 120₁, 120₂, 120₃ and 120₄, and a surgical tool 124. MPS 102 and medical imaging device 104 are coupled with database 106. Processor 108 is coupled with database 106 and display 110. MPS 102 includes plurality of MPS sensors 120₁, 120₂, 120₃, and 120₄. Medical imaging device 104 includes image
30 detector 116.

MPS 102 receives and processes data related to the position of an area of the body of a patient. It is noted that henceforth the term "position" refers to either the location or positional coordinate of a point in space, the orientation of that point in space, or both. The data is obtained via plurality of MPS sensors 120₁, 120₂, 120₃, and 120₄. MPS sensor 120₁ is attached to surgical tool 124. MPS sensor 120₂ is attached to image detector 116. MPS sensor 120₃ is generally attached to an inspected area of a patient body (referenced 130). MPS sensor 120₄ is generally attached to a known area on the surface on which the patient rests.

Each of MPS sensors 120₁, 120₂, 120₃, and 120₄ contain electromagnetic field detection elements, such as coils. MPS 102 produces predetermined electromagnetic fields, which are detected by MPS sensors 120₁, 120₂, 120₃, and 120₄, respectively. MPS 102 processes the detected electromagnetic fields, and obtains an indication of the three-dimensional position of MPS sensors 120₁, 120₂, 120₃, and 120₄. In this manner, MPS 102 determines the three-dimensional position of image detector 116, surgical tool 124, a selected area of patient body 130, and a known area on the surface on which the patient rests. It is noted that the electromagnetic transmission may be reversed, such that the field detection elements are stationary and located in MPS 102 while predetermined electromagnetic fields are produced by MPS sensors 120₁, 120₂, 120₃, and 120₄. A medical positioning system such as MPS 102 is explained further in US Patent 6,233,476 to Strommer et al entitled "Medical positioning system", which is hereby incorporated by reference.

In one embodiment of the disclosed technique, each of MPS sensors 120₁, 120₂, 120₃, and 120₄ may be an electromagnetic transducer, capable of both transmitting an electromagnetic field and detecting an electromagnetic field. In addition, MPS 102 contains at least one reference electromagnetic transducer (not shown) which is placed at a certain reference location. The reference electromagnetic transducer may be one of MPS sensors 120₁, 120₂, 120₃, and 120₄. MPS 102 further

contains an MPS processor (not shown) coupled with the reference electromagnetic transducer and each of the other electromagnetic transducers. The reference transducer then transmits predetermined electromagnetic signals in the form of electromagnetic fields, which are
5 detected by MPS sensors 120₁, 120₂, 120₃, and 120₄, respectively. Alternatively, the electromagnetic transmission is reversed, such that predetermined electromagnetic signals are transmitted by MPS sensors 120₁, 120₂, 120₃, and 120₄, respectively, and are detected by the reference transducer. The MPS processor processes the detected
10 electromagnetic signals, and obtains an indication of the three-dimensional position of MPS sensors 120₁, 120₂, 120₃, and 120₄. In this manner, MPS 102 determines the three-dimensional position of image detector 116, surgical tool 124, a selected area of patient body 130, and a known area on the surface on which the patient rests.

15 The position of image detector 116, obtained via MPS sensor 120₂, is used in determining parameters (i.e., external optical parameters) relating to medical imaging device 104. It is noted that the parameters relating to medical imaging device 104 may also be obtained by other means, such as pre-known calibration target or fiducial points and the
20 relationship of these points to their corresponding identified image.

The position of the patient body, obtained via MPS sensor 120₃, is used as a reference to compensate for arbitrary patient movement. The data from MPS sensor 120₃ is used to determine motion of the patient with respect to a known set of coordinates, such as the origin of the magnetic
25 coordinate system or with respect to another sensor, or a set plurality of sensors, such as MPS sensor 120₄. It is noted that each of MPS sensors 120₃ and 120₄ may be used individually to determine patient movement, or they may be used both together. It is further noted that either of MPS sensors 120₃ or 120₄ may include a plurality of sensors (i.e., there may be
30 a plurality of sensors attached to an inspected area of patient body 130,

and there may be a plurality of sensors attached to a known area on the surface on which the patient rests).

The process of compensating for patient movement or movement of medical imaging device 104 is known as coordinate system normalization. Coordinate system normalization, also referred herein
5 below as "normalization", is done using the corresponding reference sensors (i.e., MPS sensors 120₃ or 120₄) for compensating patient movement. Compensating for movement of medical imaging device 104 may further utilize MPS sensor 120₂ attached to image detector 116 on
10 medical imaging device 104, in addition to MPS sensors 120₃ or 120₄. It is noted that normalization allows for the utilization of data sets among different sessions or medical procedures. The term "medical procedure" refers to any type of medical procedure performed on a patient, such as diagnostic, therapeutic, or preventative procedures. A medical procedure
15 may be done in several stages. Each stage in a single medical procedure is known as a "session". It is further noted that no nullification of MPS sensor readings are required due to coordinate system normalization. All data readings obtained from MPS sensors 120₁ and 120₂ may be used for processing, with no need to dismiss a "faulty" reading as a result of
20 arbitrary patient motion. It is yet further noted that coordinate system normalization allows for representing MPS data in different coordinate systems. For example, data may be represented with respect to the coordinate system of the patient, whereby the body of the patient is stationary, and the inspected organ and the surgical tool move.
25 Alternatively, data may be represented with respect to the coordinate system of the inspected organ, whereby the inspected organ is stationary, and the body of the patient and the surgical tool move. Further alternatively, data may be represented with respect to the coordinate system of the surgical tool, whereby the surgical tool is stationary, and the
30 body of the patient and the inspected organ move.

MPS 102 may include additional MPS sensors to be used as further references, similar to MPS sensor 120₃ or MPS sensor 120₄, thereby further assisting with coordinate system normalization. It is noted however, that other methods for assigning a reference point can be used, such as initial referencing between all MPS sensors and strapping the patient during the entire medical procedure, analyzing the acquired images and identifying a recurring visual point or section therein for each of the MPS sensors other than the sensor attached to the transducer, and the like.

MPS 102 also provides data for obtaining phase information relating to the activity state of an inspected organ. For example, if the inspected organ is a heart, phase information may be heart timing signals denoting stages within a cardiac cycle. A cardiac cycle is defined as the time between two subsequent heart contractions. The electrical activity of the heart as a function of time, such as electrical timing signals obtained by an ECG monitor, can reveal the current stage or phase of the heart within the cardiac cycle. Alternatively, if the inspected organ is a lung, phase information may relate to respiratory rate and stages of the lung within a respiratory cycle. For example, if the inspected organ is an eye, phase information may relate to movement of the eyelid and related ophthalmologic features. Processor 108 obtains phase information by processing data provided by MPS 102 via MPS sensor 120₁, without the need for any external monitoring device (such as an ECG device). Other sensors may be used independently or in addition in order to generate phase information (e.g., MPS sensor 120₃ in conjunction with MPS sensor 120₁).

Medical imaging device 104 provides a two-dimensional image of an area within the body of the patient. In the example set forth herewith, the area inspected is the heart and surrounding blood vessels. Medical image device 104 can include any type of image acquisition system known in the art, such as ultra-sound, inner-vascular ultra-sound, X-ray, C-Arm

machines (equipped with such devices), fluoroscopy, angiography, computerized tomography, nuclear magnetic resonance, positron-emission tomography, single-photon-emission tomography, and the like.

Medical imaging device 104 acquires a two-dimensional image
5 via image detector 116. Image detector 116 detects a plurality of two-dimensional images, each representing a view of the inspected organ (e.g., the heart). MPS sensor 120₂ attached to image detector 116 obtains information relating to the position of image detector 116. A frame grabber (not shown) acquires the images and provides them to database 106.

10 Database 106 stores data required by system 100. Database 106 is typically a database unit, which allows for storage and access of data records. The data includes frames of captured two-dimensional images from medical imaging system 104, as well as MPS sensor readings from MPS 102. Data is transferred to database 106, from which
15 the data is recalled for processing. Intermediate and final data values obtained throughout computations of processor 108 may also be stored in database 106. Database 106 may further store information from additional devices used in conjunction with system 100 (e.g., information from an external monitoring device such as an ECG, intravascular ultrasound
20 information, and the like). In general, database 106 stores all possible information that may be needed by system 100.

Data elements that are stored in database 106 are time-tagged. The term "time-tagging" herein below refers to the process of associating a data element with the exact time at which that data element was obtained
25 (e.g., associating an MPS coordinate reading with the exact time at which that reading was obtained). The data obtained via each of plurality of MPS sensors 120₁, 120₂, 120₃ and 120₄ is time-tagged. The plurality of two-dimensional images acquired by medical imaging device 104 is also time-tagged. The time-tags are taken into account when processing the data
30 elements stored in database 106.

Latency compensation is performed on all the time-tagged data elements. In general, image frames from the set of 2D images acquired by medical imaging device 104 are shifted so that the time-tags thereof match the time-tag of the corresponding MPS data set (i.e., images
5 acquired at the same time as an MPS coordinate reading was obtained will be matched with one another).

Processor 108 operates on data gathered in database 106. Processor 108 performs necessary calculations, correlates between the different data streams, and performs filtering, segmentation, reconstruction
10 of three-dimensional models, and other operations. Processor 108 associates between captured two-dimensional images, position information relating to the respective images, and phase information relating to the respective images. Processor 108 constructs trajectories of surgical tool 124 guided within the body of a patient, respective of different
15 activity-states of an inspected organ. Processor 108 may further construct a three-dimensional image from captured two-dimensional images having the same activity-state, and from three-dimensional position data associated with each of the images.

Display 110 presents a motion picture, or image sequence, of
20 the inspected organ in real-time. The motion picture consists of the two-dimensional images captured by medical imaging device 104, with the three-dimensional position data of surgical tool 124 obtained by MPS 102 superimposed via optical projection. The motion picture may consist of a projection of a constructed three-dimensional model of the organ. The
25 motion picture displays the trajectory of surgical tool 120 as the surgical tool is guided within the patient body, respective of different activity-states of an inspected organ. Display 110 may present a selected image frame of the motion picture respective of the real-time detected organ activity-state. Display 110 may provide different playback effects, freeze frames, change
30 speed, select features, and the like. For example, display 110 may present a playback of previous images in a sequence, showing the progress of

surgical tool during previous activity states of the organ. Display 110 may include multiple monitors, or separate windows within a single monitor, where each monitor or window presents a different view. For example, one monitor or window presents the current real-time three-dimensional position data of surgical tool 124 superimposed on the current image frame of the inspected organ respective of the current activity-state, while another monitor or window presents the current real-time three-dimensional position data of surgical tool 124 superimposed on a previous image frame (or image sequence) of the inspected organ respective of a previous activity-state (or activity-states). Display 110 may be a two-dimensional display, an auto-stereoscopic display to be viewed with a suitable pair of spectacles, a stand alone stereoscopic display, a pair of goggles, and the like.

Reference is now made to Figure 2, which is a block diagram of a method for registering three-dimensional magnetic coordinates into two-dimensional optical coordinates, operative in accordance with another embodiment of the disclosed technique.

In procedure 210, a transformation model for magnetic-optical correlation is determined. Magnetic-optical correlation involves the conversion of three-dimensional magnetic coordinates, obtained from MPS sensors, into three-dimensional optical coordinates. The correlation procedure is generally performed once, during the initialization of the entire system. Procedure 210 involves defining a transformation model between the magnetic coordinate system and the optical coordinate system. This transformation defines a global solution of the working volume and does not require any further manual calibration or correlation. In general, as long as there is no change in the magnetic configuration parameters, correlation need not be repeated. The correlation may be modified automatically during the medical procedure in order to calibrate minor changes between the magnetic and optical coordinate systems.

In procedure 220, a transformation model for optical projection is determined. Optical projection involves the conversion of three-dimensional optical coordinates (obtained using magnetic-optical correlation) into two-dimensional optical coordinates, to be superimposed
5 on an image displayed by display 110. Optical projection is based on a transformation model from a three-dimensional coordinate system to a two-dimensional coordinate system. This transformation model is based on external optical parameters, internal optical parameters, and image distortion parameters of medical imaging device 104. Procedure 220
10 consists of procedures 222, 224, 226, and 228.

In procedure 222, external optical parameters are determined. External optical parameters relate to the position of the medical imaging device 104. In particular, external optical parameters define the coordinate system of medical imaging device 104 with respect to the defined optical
15 coordinate system. In procedure 224, internal optical parameters are determined. Internal optical parameters of the medical imaging device 104 relate to the image acquisition mechanism. For example, internal optical parameters may include: lens center point, focal length and the like. In procedure 226, image distortion parameters are determined. Image
20 distortion parameters relate to parameters which alter the original proportion of objects as they appear in the images acquired by medical imaging device 104, as a result of physical characteristics of the image acquisition mechanism and the way that the image acquisition mechanism operates. Image distortion parameters may be computed either as a part
25 of the internal optical parameters or as an additional set of correction parameters.

It is noted that the external optical parameters are usually calculated continuously in real-time, whereas it is generally sufficient to compute the internal optical parameters and image distortion parameters
30 once during the beginning stages of the medical procedure. However, there may be cases when it is necessary to re-calculate the internal optical

parameters and image distortion parameters at a later stage. MPS data may also be used in re-calculating the external optical parameters, internal optical parameters, and image distortion parameters of medical imaging device 104. In procedure 228, a transformation between the three-dimensional coordinate system and two-dimensional coordinate system is defined based on external optical parameters, internal optical parameters, and image distortion parameters of medical imaging device 104.

Alternatively, or in addition, a direct translation between the 3D MPS coordinate system and the image plane 2D coordinate system can be determined based on known MPS coordinate readings and their relationship to their corresponding identified image coordinates. It is noted that projection procedure 220 takes into account the time-tagged data from the reference sensors of the MPS data to be projected and the images to be projected upon. In case patient movement occurred after an image was acquired, or in case movement of medical imaging device 104 occurred after MPS data was taken, the reference sensors are used in order to compensate for either movements and ensure that the MPS data is projected accurately.

The method of Figure 2 also includes procedures for converting a set of three-dimensional magnetic coordinates to two-dimensional optical coordinates, shown with reference to the dashed lines. Three-dimensional magnetic coordinates representing position data is obtained from MPS 102. In procedure 230, magnetic-optical correlation is applied to three-dimensional magnetic coordinates to produce the equivalent three-dimensional optical coordinates. In procedure 240, optical projection is applied to the three-dimensional optical coordinates to produce the equivalent two-dimensional optical coordinates. Alternatively a direct transformation from the MPS coordinate system to the image plane can be used. The two-dimensional optical coordinates may be shown on display 110, in context of the appropriate image frame of the motion picture. The

MPS data is projected onto the image plane including all the needed distortion and conversions which affect the projection coordinates only.

Reference is now made to Figure 3, which is a block diagram of a method for obtaining phase information from MPS data sets, operative in accordance with a further embodiment of the disclosed technique. In procedure 302, data sets are obtained from MPS 102. Each MPS data set comprises a series of position coordinate readings of image detector 116, surgical tool 124, a selected area of patient body 130, or a known area on the surface on which the patient rests, respectively, as received from one of plurality of MPS sensors 120₁, 120₂, 120₃ and 120₄. MPS 102 processes detected electromagnetic fields to obtain the respective position coordinate readings, which are subsequently stored in database 106. It is recalled that each MPS sensor position coordinate reading is time-tagged, or associated with the exact time at which the reading was obtained. Thus, each MPS data set received from MPS sensor 120₁ comprises a collection of coordinate readings demonstrating the precise motion trajectory of surgical tool 124 over time.

In procedure 318, cardiac phase information is obtained from cardiac motion. In particular, cardiac phase information is obtained from data streams originating from MPS sensor 120₁ located on surgical tool 124. Procedure 318 consists of procedures 304, 306, 310, 314 and 316.

In procedure 304, periodic motion frequencies are detected and identified in a time-tagged MPS data set. As surgical tool 124 is guided inside a vessel within the body of a patient, the motion of surgical tool 124 is influenced by two additional factors. The first factor relates to activity of the heart, or cardiac motion, such as systole and diastole. Cardiac motion affects the vessel in a certain way, such as contraction or expansion in varying degrees and at periodic intervals. The second factor relates to breathing activity, or respiratory motion, such as inhaling and exhaling. Respiratory motion affects the vessel in a certain way, such as contraction or expansion in varying degrees and at periodic intervals. Taken together,

the overall motion of surgical tool 124 is composed of the cardiac motion and the respiratory motion superimposed onto the basic guiding movement (which corresponds to the vessel topography). The term "organ timing signal" refers herein below to the movement of the blood vessel
5 arising from the periodic motion frequencies (i.e., the cardiac motion and the respiratory motion together).

Since the cardiac motion and respiratory motion are cyclic in nature, the periodic frequencies can be detected in the overall trajectory of surgical tool 124. The specific frequencies relating to the cardiac motion
10 exhibit different characteristics than the specific frequencies relating to the respiratory motion. The specific frequencies relating to the cardiac motion are identified from the detected periodic frequencies. Similarly, the specific frequencies relating to the respiratory motion are identified from the detected periodic frequencies. Processor 108 performs the analysis on the
15 MPS data set and identifies the relevant periodic motion frequencies.

In procedure 306, periodic motion frequencies are filtered from the time-tagged MPS data set. The periodic motion frequencies detected in procedure 304 are separated out from the overall trajectory of surgical tool 124. The remaining motion components correspond to the central axis
20 of the guiding motion of surgical tool 124, which represents the vessel topography, or "centerline trajectory" (referenced procedure 308). The time-tags associated with the MPS data set are retained for each of the filtered periodic motion frequencies. Processor 108 filters out the relevant periodic motion frequencies from the MPS data set.

25 In procedure 310, the mechanical movement of the vessel originating from the cardiac motion, or "cardiac trajectory", is reconstructed from the MPS data sets and the filtered periodic motion frequencies. In particular, the cardiac trajectory is reconstructed according to the previously identified specific frequencies relating to the cardiac motion.
30 The reconstructed cardiac trajectory may be reflected, for example, by a graph that indicates the trajectory of the vessel due to cardiac motion over

a period of time. Processor 108 analyzes the relevant periodic motion frequencies and creates a reconstruction of the cardiac trajectory.

In procedure 312, the mechanical movement of the vessel originating from the respiratory motion, or "respiratory trajectory", is reconstructed from the MPS data sets and the filtered periodic motion frequencies. In particular, the respiratory trajectory is reconstructed according to the previously identified specific frequencies relating to the respiratory motion. The reconstructed respiratory trajectory may be reflected, for example, by a graph that indicates the trajectory of the vessel due to respiratory motion over a period of time. Processor 108 analyzes the relevant periodic motion frequencies and creates a reconstruction of the respiratory trajectory.

Reconstruction of the respiratory trajectory may be based solely on coordinate readings obtained from the external reference sensors (i.e., MPS sensors 120₃ or 120₄). It is noted that an additional reference sensor (or plurality thereof) may be attached (i.e., externally or internally) to the body of the patient, to monitor breathing patterns and the like. For example, an intravascular sensor may be used for this purpose. This sensor functions as a confirmation mechanism to provide support data regarding respiratory motion, and more accurately determine periodic motion frequencies relating to respiratory motion. It is noted that the same or additional sensor (or plurality thereof) may be used for gathering additional cardiac data either as a confirmation mechanism and/or for providing supporting data for cardiac phase detection.

In procedure 314, phase detection is performed on the reconstructed cardiac trajectory. The cardiac trajectory consists of different phases or activity-states of the heart, corresponding to different points within a cardiac cycle. The phases repeat themselves periodically with each cycle. The plurality of cardiac activity-states is identified on the reconstructed cardiac trajectory during phase detection. Processor 108

performs the analysis of the cardiac trajectory and identifies the different cardiac cycle phases.

Reference is now made to Figure 4A, which is a schematic illustration of a sample cardiac trajectory, in electrical signal representation and in mechanical signal representation. The mechanical signal representation of the cardiac trajectory, generally referenced 400, includes a plurality of cardiac activity-states (i.e., cardiac cycle phases), such as activity-states T_1 , T_2 and T_3 , in each of plurality of cardiac cycles 410, 420 and 430. The mechanical representation of the cardiac trajectory is equivalent to the cardiac trajectory reconstructed from the MPS data sets and the filtered periodic motion frequencies in procedure 310. The electrical signal representation of the cardiac trajectory, generally referenced 450, depicts the same activity-states T_1 , T_2 and T_3 , in each of plurality of cardiac cycles 410, 420 and 430. However the precise time at which these activity-states occur may be different in the two representations, as there is a slight delay at the electrical representation with respect to the mechanical representation. For example, it is shown that activity-state T_1 of cardiac cycle 430 occurs at time t_A in cardiac trajectory 400 and at time t_B in cardiac trajectory 450. Therefore, it is necessary to perform an alignment between the activity states, when using information from the electrical representation for phase detection. The electrical representation of the cardiac trajectory is equivalent to the electrical timing signals obtained by an ECG monitor.

It is noted that the detection of cardiac phases is performed based solely on data sets originating from at least MPS sensor 120₁ located on surgical tool 124, and perhaps also from the reference sensors (i.e., MPS sensors 120₃ and 120₄). These data sets provide a mechanical representation of the cardiac trajectory. No external monitoring device is required to obtain cardiac phase information. It is noted that periodic motion components relating to the respiratory motion may also be used as supporting data for cardiac phase detection. It is further noted that phase

detection may be performed on the original MPS data sets, rather than on the reconstructed cardiac trajectory, using the detected and filtered periodic motion frequencies. In this case, the different phases or activity-states of the heart are identified directly on the MPS data sets obtained in
5 procedure 302.

In procedure 316, cardiac phase information is associated with the MPS data sets. Each data set obtained from MPS sensor 120₁ relating to position of surgical tool 124 is matched to one of plurality of activity-states T_1 , T_2 and T_3 , according to their corresponding time elements (i.e.,
10 time-tags). The position of the inspected vessel, and consequently the position of guided surgical tool 124, is different during different activity-states of the inspected organ. Processor 108 associates between a coordinate reading and the matching phase thereof, and stores the information in database 106.

15 Respiratory phase information may be obtained from the respiratory motion, in a similar manner as cardiac phase information is obtained from the cardiac motion. Respiration activity-states may be identified on the reconstructed respiratory trajectory using the periodic motion components relating to the respiratory motion. Periodic motion
20 components relating to the respiratory motion may also be used in correlation of non-corresponding data sets (discussed with reference to Figure 8).

Respiratory phase information is obtained from respiratory motion in optional procedure 320. Procedure 320 consists of procedures
25 304, 306, 312, 322 and 324. In procedure 312, the respiratory trajectory is reconstructed from the MPS data sets and the filtered periodic motion frequencies, as elaborated upon earlier. In procedure 322, phase detection is performed on the reconstructed respiratory trajectory. Similar to the cardiac trajectory, the respiratory trajectory consists of different
30 phases or activity-states of the lungs, corresponding to different points within a respiratory cycle. The respiratory activity-states of the lungs may

be identified from the phases of the respiratory trajectory. The phases repeat themselves periodically with each cycle. The plurality of respiratory activity-states is identified on the reconstructed respiratory trajectory during phase detection. Processor 108 performs the analysis of the
5 respiratory trajectory and identifies the different respiratory cycle phases.

Reference is now made to Figure 4B, which is a schematic illustration of a sample respiratory trajectory in mechanical signal representation. The mechanical signal representation of the respiratory trajectory, generally referenced 460, includes a plurality of respiratory
10 activity-states (i.e., respiratory cycle phases), such as activity-states T_4 , T_5 and T_6 . The mechanical representation of the respiratory trajectory is equivalent to the respiratory trajectory reconstructed from the MPS data sets and the filtered periodic motion frequencies in procedure 310.

It is noted that the detection of respiratory phases is performed
15 based solely on data sets originating from MPS sensor 120₁ located on surgical tool 124, and from MPS sensors 120₃ and 120₄, located on a selected area of patient body 130, and a known area on the surface on which the patient rests, respectively. These data sets provide a mechanical representation of the respiratory trajectory. No external
20 monitoring device is required to obtain respiratory phase information. It is further noted that phase detection may be performed on the original MPS data sets, rather than on the reconstructed respiratory trajectory, using the detected and filtered periodic motion frequencies. In this case, the different phases or activity-states of the lung are identified directly on the MPS data
25 sets obtained in procedure 302.

It is noted that the actual value of the cardiac rate or respiratory rate of the patient may be obtained without the use of an external monitoring device (such as an ECG device). The cardiac rate or respiratory rate of the patient may be obtained solely from MPS sensors
30 120₁, 120₃ and 120₄, either individually or jointly.

In procedure 324, respiratory phase information is associated with the MPS data sets. Each data set obtained from MPS sensor 120₁ relating to position of surgical tool 124 is matched to one of plurality of activity-states T₄, T₅ and T₆, according to their corresponding time tags.

5 Procedure 324 is analogous to procedure 316 discussed above.

Reference is now made to Figure 5, which is a schematic illustration of a trajectory of the surgical tool of the system of Figure 1, inside a vessel in the body of a patient, respective of different activity-states of the cardiac trajectory of Figure 4. At activity-state T₁ of each of the cardiac cycles 410, 420 and 430, the position of the vessel is represented by a vessel image 570 (indicated in Figure 5 with solid lines). At activity-state T₂ of each of the cardiac cycles 410, 420 and 430, the position of the vessel is represented by a vessel image 572 (indicated in Figure 5 with dashed lines). At activity-state T₃ of each of the cardiac cycles 410, 420 and 430, the position of the vessel is represented by a vessel image 574 (indicated in Figure 5 with dotted lines). Thus, each of the coordinates 552, 554, 556, 558, 560, 562, 564, 566 and 568 corresponds to a position of surgical tool 124, while the vessel is at a different position, in a different activity-state of a cardiac cycle.

20 For example, coordinate 552 corresponds to activity-state T₁ in cardiac cycle 410, meaning that when MPS sensor 120₁ on surgical tool 124 is at coordinate 552, the heart of the patient is at activity-state T₁. Coordinate 554 corresponds to activity-state T₂ in cardiac cycle 410, meaning that when MPS sensor 120₁ on surgical tool 124 is at coordinate 554, the heart of the patient is at activity-state T₂. Coordinate 556 corresponds to activity-state T₃ in cardiac cycle 410, meaning that when MPS sensor 120₁ on surgical tool 124 is at coordinate 556, the heart of the patient is at activity-state T₃. Coordinate 558 corresponds to activity-state T₁ in cardiac cycle 420. Coordinate 560 corresponds to activity-state T₂ in cardiac cycle 420. Coordinate 562 corresponds to activity-state T₃ in cardiac cycle 420. Coordinate 564 corresponds to activity-state T₁ in

cardiac cycle 430. Coordinate 566 corresponds to activity-state T_2 in cardiac cycle 430. Coordinate 568 corresponds to activity-state T_3 in cardiac cycle 430. It is noted that coordinates 552, 554, 556, 558, 560, 562, 564, 566 and 568 are related to the respiratory activity states T_4 , T_5 , T_6 in a similar manner.

According to another aspect of the disclosed technique, position measurements, together with acquired images, are processed with respect to the activity-state of the inspected organ at the time of acquisition or measurement. For example, with reference to Figure 1, display 110 displays the trajectory of a surgical tool 124 superimposed on a two-dimensional image of an inspected organ, wherein the two-dimensional image corresponds to an activity-state determined by the current position of surgical tool 124 inside the inspected organ. The system records the path which surgical tool 124 follows inside the inspected organ, in either a forward or a backward direction. The system further registers this path with monitored activity-states of the inspected organ and with the instantaneous position of surgical tool 124.

Reference is now made to Figure 6, which is a schematic illustration of trajectories of a guided surgical tool inside a vessel in the body of a patient, each trajectory processed with respect to a different activity-state. For example, processor 108 associates for a given two-dimensional image acquired during activity-state T_1 , all the position coordinate readings of surgical tool 124 (i.e., coordinates 612, 618 and 624) which were detected during activity-state T_1 at any cycle of cardiac trajectory 400. Similarly, processor 108 associates for a given two-dimensional image acquired during activity-state T_2 , all the position coordinate readings (i.e., coordinates 614, 620 and 626) which were detected during activity-state T_2 at any cycle of cardiac trajectory 400; and further associates for a given two-dimensional image acquired during activity-state T_3 , all the position coordinate readings (i.e., coordinates 616,

622 and 628) which were detected during activity-state T_3 at any cycle of cardiac trajectory 400.

Processor 108 calculates a trajectory 606 from points 612, 618 and 624, associated with activity state T_1 . Similarly, processor 108
5 calculates a trajectory 608 from points 614, 620 and 626 associated with activity state T_2 , and further calculates a trajectory 610 from points 616, 622 and 628 associated with activity state T_3 .

Processor 108 associates between each of the calculated trajectories and a two-dimensional image, respective of a given organ
10 activity-state. Processor 108 associates between trajectory 612 and two-dimensional image 600 (indicated with solid lines), respective of activity state T_1 . Similarly, processor 108 associates between trajectory 614 and two-dimensional image 602 (indicated with dashed lines), respective of activity state T_2 and further between trajectory 614 and two-dimensional
15 image 604 (indicated with dotted lines), respective of activity state T_3 .

Display 110 presents a superimposition of each of the calculated trajectories on its respective two-dimensional image. For example, display 110 presents trajectory 606 superimposed on two-dimensional image 600, trajectory 608 superimposed on two-dimensional image 602 and trajectory
20 610 superimposed on two-dimensional image 604. Display 110 may present these images as a single image frame shown one at a time, or a sequence of images (i.e., motion picture) shown consecutively.

It is noted that points 612, 614, 616, 618, 620, 622, 624, 626 and 628 represent a situation similar to that presented by points 552, 554,
25 556, 558, 560, 562 564, 566 and 568 with respect to Figure 5. However, according to an aspect of the disclosed technique presented in Figure 6, processor 108 calculates a trajectory of surgical tool 124 based on the position coordinate readings detected during a given activity-state. Thus, each trajectory corresponds to a different activity-state of the inspected
30 organ. Processor 108 further associates each calculated trajectory with a vessel image acquired during the corresponding activity-state.

Reference is now made to Figure 7, which is a block diagram of a method for superimposing MPS data onto two-dimensional image data for corresponding data sets, operative in accordance with another embodiment of the disclosed technique. It is recalled that the position coordinate readings obtained from MPS 102 is time-tagged. Similarly, the sequence of two-dimensional images obtained from medical imaging device 104 is time-tagged. "Corresponding data sets" refer to a pair of data sets which have the same time-tags. It is noted that the time-tag of a data set refers to the set of time-tags of the elements within the data set.

For example, an MPS data set is corresponding with a two-dimensional images data set if readings in the MPS data set have the same time-tag as images in the two-dimensional images data set. Corresponding data sets represent data sets that occur during the same session in a medical procedure. "Non-corresponding data sets" refer to a pair of data sets which have different time-tags. For example, an MPS data set is non-corresponding with a two-dimensional images data set if readings in the MPS data set have a different time-tag than all the images in the two-dimensional images data set. Non-corresponding data sets represent data sets that were recorded during different sessions (within the same or different medical procedures).

In procedure 702, an MPS data set is normalized. The MPS data set, which comprises three-dimensional coordinate readings in the magnetic coordinate system, is obtained from MPS 102. Normalization compensates for patient movement or movement of medical imaging device 116, as discussed with reference to Figure 1. Normalization is performed using MPS data with corresponding time-tags from the reference sensors (i.e., MPS sensors 120₃ or 120₄), and perhaps also MPS sensor 120₂ as well.

In procedure 704, magnetic-optical correlation is performed on the normalized MPS data set. The correlation procedure transforms the three-dimensional position magnetic coordinate into a three-dimensional

coordinate in the optical coordinate system. The correlation procedure is based on the magnetic-optical transformation model, determined in procedure 210 with reference to Figure 2.

In procedure 706, optical projection is performed on the correlated MPS data set. The optical projection procedure transforms the three-dimensional position MPS coordinate reading in the optical coordinate system to a two-dimensional coordinate. The optical projection procedure is based on the three-dimensional to two-dimensional optical transformation model, determined in procedure 228 with reference to Figure 2. It is noted that the three-dimensional to two-dimensional optical transformation model is a function of certain parameters (i.e., internal and external optical parameters and image distortion parameters of medical imaging device 104), which are computed at a given instant in time, and as such, is time-tagged. Therefore the optical projection procedure is based on a three-dimensional to two-dimensional optical transformation model which has the same time-tag as the MPS data set.

A direct transformation between 3D MPS data to 2D image coordinates can be used in case such a direct translation was computed. Compensation for optical distortions is done at a given instant in time and as such, is time-tagged.

In procedure 708, the MPS data set is superimposed onto an image from the two-dimensional images data set. The two-dimensional images data set is obtained from medical imaging device 104. The MPS data set now includes two-dimensional position coordinates in the optical coordinate system. With reference to Figure 1, processor 108 associates between a position coordinate reading and a two-dimensional image, in accordance with their mutual time-tag. Display 110 may present a picture showing the position of surgical tool 124 respective of the inspected organ, at a given point in time, in accordance with acquired two-dimensional image data and acquired MPS data. Further, as will be elaborated upon with reference to Figures 9 and 10, display 110 may present a motion

picture showing the trajectory of the guided surgical tool respective of the inspected organ, in accordance with acquired two-dimensional image data set and acquired MPS data set.

The MPS data and two-dimensional image data may further be
5 associated with activity state information. With reference to Figure 1, processor 108 associates between a position coordinate reading and a two-dimensional image, in accordance with their mutual time-tag, respective of a given organ activity-state. Display 110 may present an image frame showing the position of surgical tool 124, respective of the
10 inspected organ at a given activity-state, in accordance with acquired two-dimensional image data, acquired MPS data, and associated activity-state information. Further, display 110 may present a motion picture showing the trajectory of the guided surgical tool respective of the inspected organ at a given activity-state, in accordance with acquired two-dimensional
15 image data set, acquired MPS data set, and associated activity-state information. This will be elaborated upon with reference to Figures 9 and 10.

Reference is now made to Figure 8, which is a block diagram of a method for superimposing MPS data onto two-dimensional image data
20 for non-corresponding data sets, operative in accordance with a further embodiment of the disclosed technique. A first MPS data set with a first time-tag is corresponding with a two-dimensional images data set. A second MPS data set with a second time-tag is non-corresponding with the two-dimensional images data set. The time-tagged MPS data sets are
25 obtained from MPS 102. The time-tagged two-dimensional images data set is obtained from medical imaging device 104.

In procedure 318, cardiac phase information is obtained from cardiac motion data, for both the first MPS data set and the second MPS data set. Procedure 318 involves detecting and identifying periodic motion
30 frequencies, filtering periodic motion components, reconstructing the cardiac trajectory from the MPS data set and filtered periodic motion

frequencies, performing phase detection on the reconstructed cardiac trajectory, and associating each coordinate reading in the MPS data set with a cardiac phase, in accordance with their time-tags. Periodic motion components relating to the respiratory motion may also be used as supporting data for cardiac phase detection. Procedure 318 is described in detail with respect to Figure 3.

In procedure 320, respiratory phase information is obtained from respiratory motion data, for both the first MPS data set and the second MPS data set. It is noted that procedure 320 is optional, and may be performed instead of procedure 318, or in conjunction with procedure 318. Procedure 320 involves detecting and identifying periodic motion frequencies, filtering periodic motion components, reconstructing the respiratory trajectory from the MPS data set and filtered periodic motion frequencies, performing phase detection on the reconstructed respiratory trajectory, and associating each coordinate reading in the MPS data set with a respiratory phase, in accordance with their time-tags. Procedure 320 is described in detail with respect to Figure 3.

In procedure 820, a third MPS data set with the same time-tag as the first MPS data set is generated from the second MPS data set, using phase alignment between the phases of the two MPS data sets. In particular, the coordinate readings of the second MPS data set are assigned the same time-tags as the coordinate readings of the first MPS data set, by matching the phases of the coordinate readings from each data set. Each of the detected phases in the second MPS data set is mapped to the matching phase in the first MPS data set. Each of the detected phases in the second MPS data set (and thus each coordinate reading associated with that phase) is then assigned a new time-tag based on the time-tag of the matching phase in the first MPS data set. For example, if phase A occurs at time "x" in the second MPS data set, and phase A occurs at time "y" in the first MPS data set, then phase A is reassigned time-tag "y" in the third MPS data set. The phase mapping

aligns the phases of the cardiac trajectory of the second data set with the cardiac trajectory of the first MPS data set. After the procedures of mapping and reassigning have been completed, the resulting data set will have the same time-tag as the first MPS data set, and hence as the two-dimensional image data set. Therefore, the third MPS data set will be corresponding with the two-dimensional image data set. It is noted that periodic motion components relating to the respiratory motion may be used in addition to, or instead of, the periodic motion components relating to the cardiac motion, for performing phase alignment. It is noted that procedure 820 may generate simply an index of each element in the third data set.

In procedure 822, magnetic-optical correlation is performed on the third MPS data set. It is noted that normalization, or compensating for patient movement or movement of medical imaging device 116, is performed prior to procedure 822. Normalization is discussed in procedure 702 with reference to Figure 7. Normalization may be performed immediately prior to procedure 820 or immediately after procedure 820. The correlation procedure transforms the three-dimensional position magnetic coordinate into a three-dimensional coordinate in the optical coordinate system. The correlation procedure is based on the magnetic-optical transformation model, determined in procedure 210 with reference to Figure 2.

In procedure 824, optical projection is performed on the correlated third MPS data set. The optical projection procedure transforms the three-dimensional position MPS coordinate in the optical coordinate system to a two-dimensional optical coordinate. The optical projection procedure is based on the three-dimensional to two-dimensional optical transformation model, determined in procedure 228 with reference to Figure 2. It is recalled that the three-dimensional to two-dimensional optical transformation model is time-tagged. Therefore the optical projection procedure is based on a three-dimensional to two-dimensional

optical transformation model which has the same time-tag as first MPS data set.

In procedure 826, the third MPS data set is superimposed onto an image from the two-dimensional images data set. With reference to
5 Figure 1, processor 108 associates between a position coordinate reading in the third MPS data set and a two-dimensional image, in accordance with their mutual time-tag. Display 110 may present an image frame showing the position of surgical tool 124 respective of the inspected organ, at a given point in time, in accordance with acquired two-dimensional image
10 data and acquired MPS data. Further, display 110 may present a motion picture showing the trajectory of the guided surgical tool respective of the inspected organ, in accordance with acquired two-dimensional image data set and acquired MPS data set. The MPS data and two-dimensional image data may further be associated with activity state information. Display 110
15 may further simultaneously present MPS data with a corresponding data set and with a non-corresponding data set. For example, presenting a superimposition of current real-time MPS data on current real-time images (i.e., corresponding data sets), while at the same time presenting a superimposition of the same current real-time MPS data on previously
20 taken images (i.e., non-corresponding data sets) using associated activity state information.

Reference is now made to Figure 9, which is a block diagram of a method for constructing trajectories of a guided surgical tool within the body of a patient, respective of different activity-states of an inspected
25 organ (e.g., such as shown in Figure 6), operative in accordance with another embodiment of the disclosed technique. In the following example, an MPS data set corresponding with a two-dimensional image data set is used. It is noted that non-corresponding data sets may be used as well, after simply undergoing phase alignment, similar to procedure 820
30 discussed with reference to Figure 8. The time-tagged MPS data set is

obtained from MPS 102. The time-tagged two-dimensional images data set is obtained from medical imaging device 104.

In procedure 318, cardiac phase information is obtained from cardiac motion data, for the MPS data set. Procedure 318 involves
5 detecting and identifying periodic motion frequencies, filtering periodic motion components, reconstructing the cardiac trajectory from the MPS data set and filtered periodic motion frequencies, performing phase detection on the reconstructed cardiac trajectory, and associating each
10 coordinate reading in the MPS data set with a phase, in accordance with their time-tags. Periodic motion components relating to the respiratory motion may also be used as supporting data for cardiac phase detection. Procedure 318 is described in detail with respect to Figure 3.

In procedure 320, respiratory phase information is obtained from respiratory motion data, for both the first MPS data set and the second
15 MPS data set. It is noted that procedure 320 is optional, and may be performed instead of procedure 318, or in conjunction with procedure 318. Procedure 320 involves detecting and identifying periodic motion frequencies, filtering periodic motion components, reconstructing the
20 respiratory trajectory from the MPS data set and filtered periodic motion frequencies, performing phase detection on the reconstructed respiratory trajectory, and associating each coordinate reading in the MPS data set with a respiratory phase, in accordance with their time-tags. Procedure 320 is described in detail with respect to Figure 3.

In procedure 908, correlated phase information is obtained for
25 the two-dimensional images data set. The phase information is correlated in the sense that the phase information is not obtained directly from the images but from correlated MPS data (occurring at the same time as a given image). The phases or activity-states of the heart, such as activity-states T_1 , T_2 and T_3 with reference to Figure 4, during which each two-
30 dimensional image was acquired, is identified. Identification of the activity-

states makes use of the time-tags taken during acquisition of all the images, and the phases of an MPS data set having the same time-tags.

A monitoring device such as an ECG may be used in conjunction with MPS data to obtain phase information of the two-dimensional image data set in certain instances. For example, if there was
5 no sensor within the body of the patient during acquisition of a given image (e.g., during the very beginning of the medical procedure when medical images are taken before the guide wire is inserted into the vessel), information from the monitoring device may be used together with non-
10 corresponding MPS data. In such a case, phase alignment is performed between the mechanical representation based phase data obtained by the MPS data and the external phase obtained by the monitoring device (such as electrical representation based phase data obtained from an ECG device). Phase alignment between the mechanical and electrical based
15 data is necessary in order to account for different latencies originating from the different sampled signals that represent the same cardiac trajectory. It is noted that data obtained from the monitoring device is also time-tagged.

In procedure 910, a separate MPS data set is generated for
20 each two-dimensional image, in accordance with the image phase and time-tags. All the MPS position coordinate readings acquired during the same phase are combined into a single data set. After procedure 910 has been completed, every image of the two-dimensional image data set has a corresponding MPS data set containing therein only those coordinate
25 readings which were acquired in the same phase as that image.

In procedure 912, magnetic-optical correlation is performed on each MPS data set generated in procedure 910. It is noted that normalization, or compensating for patient movement or movement of medical imaging device 116, is performed prior to procedure 912.
30 Normalization is discussed in procedure 702 with reference to Figure 7. Normalization may be performed immediately prior to procedure 910 or

immediately after procedure 910. The correlation procedure transforms the three-dimensional position magnetic coordinate into a three-dimensional coordinate in the optical coordinate system. The correlation procedure is based on the magnetic-optical transformation model, determined in
5 procedure 210 with reference to Figure 2.

In procedure 914, optical projection is performed on each correlated MPS data set generated in procedure 910. The optical projection procedure transforms the three-dimensional position MPS coordinate in the optical coordinate system to a two-dimensional optical
10 coordinate. The optical projection procedure is based on the three-dimensional to two-dimensional optical transformation model, determined in procedure 228 with reference to Figure 2. It is recalled that the three-dimensional to two-dimensional optical transformation model is time-tagged. Therefore the optical projection procedure is based on a three-
15 dimensional to two-dimensional optical transformation which has the same time-tag as the MPS data set.

In procedure 916, each MPS data set generated in procedure 910 is superimposed onto the corresponding two-dimensional image. For each two-dimensional image, the MPS coordinate readings which were
20 acquired during the same phase at the two-dimensional image are superimposed onto that image. The coordinate readings are then connected together by lines, thereby composing a spline representing the trajectory of surgical tool 124 respective of an activity state of the inspected organ. Display 110 may present an image frame showing the
25 position of surgical tool 124 respective of the inspected organ, at a given point in time, in accordance with acquired two-dimensional image data and acquired MPS data. Further, display 110 may present a motion picture showing the trajectory of the guided surgical tool respective of the inspected organ, in accordance with acquired two-dimensional image data
30 set and acquired MPS data set. The MPS data and two-dimensional image data may further be associated with activity state information. Display 110

may further simultaneously present a superimposition of current real-time MPS data on current real-time images, while presenting a superimposition of the same current real-time MPS data on previously taken images, using associated activity state information.

5 Reference is now made to Figure 10, which is a block diagram of an additional method for constructing trajectories of a guided surgical tool within the body of a patient, respective of different activity-states of an inspected organ, operative in accordance with a further embodiment of the disclosed technique. In the following example, an MPS data set
10 corresponding with a two-dimensional image data set is used. It is noted that non-corresponding data sets may be used as well, after simply undergoing phase alignment, similar to the procedure discussed with reference to Figure 8. A time-tagged MPS data set is obtained from MPS 102. A time-tagged two-dimensional images data set is obtained from
15 medical imaging device 104.

 In procedure 318, cardiac phase information is obtained from cardiac motion data, for the MPS data set. Procedure 318 involves detecting and identifying periodic motion frequencies, filtering periodic motion components, reconstructing the cardiac trajectory from the MPS
20 data set and filtered periodic motion frequencies, performing phase detection on the reconstructed cardiac trajectory, and associating each coordinate reading in the MPS data set with a phase, in accordance with their time-tags. Periodic motion components relating to the respiratory motion may also be used as supporting data for cardiac phase detection.
25 Procedure 318 is described in detail with respect to Figure 3.

 In procedure 320, respiratory phase information is obtained from respiratory motion data, for both the first MPS data set and the second MPS data set. It is noted that procedure 320 is optional, and may be performed instead of procedure 318, or in conjunction with procedure 318.
30 Procedure 320 involves detecting and identifying periodic motion frequencies, filtering periodic motion components, reconstructing the

respiratory trajectory from the MPS data set and filtered periodic motion frequencies, performing phase detection on the reconstructed respiratory trajectory, and associating each coordinate reading in the MPS data set with a respiratory phase, in accordance with their time-tags. Procedure
5 320 is described in detail with respect to Figure 3.

In procedure 1004, the centerline trajectory is reconstructed. After the periodic motion components are separated out from the overall trajectory of surgical tool 124, the remaining motion components corresponds to the central axis of the guiding motion of surgical tool 124,
10 or centerline trajectory. Procedure 1004 is similar to procedure 308 with reference to Figure 3.

In procedure 1010, separate centerline trajectories are reconstructed for each phase. Based on the time-tags and the detected phases of the cardiac trajectory, the centerline positions are matched
15 according to phase, and a different trajectory is built for each phase.

In procedure 1012, correlated phase information is obtained for the two-dimensional images data set. The phase is correlated in the sense that the phase information is not obtained directly from the images but from correlated MPS information (occurring at the same time as a given
20 image). The phases or activity-states of the heart, such as activity-states T_1 , T_2 and T_3 , with reference to Figure 4, during which each two-dimensional image was acquired, is identified. Identification of the activity-states makes use of the time-tags taken during acquisition of all the images, and the phases of an MPS data set having the same time-tags. A
25 monitoring device such as an ECG may be used in conjunction with MPS data to obtain phase information of the two-dimensional image data set in certain instances, as discussed with reference to Figure 9. In such a case, phase alignment is done between the mechanical based phase data and the electrical based phase data in order to account for different latencies
30 originating from the different sampled signals that represent the same

cardiac trajectory. Procedure 1012 is similar to procedure 908 with reference to Figure 9.

In procedure 1014, each centerline trajectory is shifted by superimposing the matching periodic motion components, for each phase
5 of the images in two-dimensional images data set. The periodic motion components, relating to cardiac motion and respiratory motion, are added on to the centerline trajectories. For each separate centerline trajectory, respective of a given phase, the periodic motion components of that phase are added onto the centerline trajectory. Each centerline trajectory is then
10 shifted, in accordance with the added periodic motion components.

In procedure 1016, magnetic-optical correlation is performed on each cardiac trajectory shifted in procedure 1014. It is noted that normalization, or compensating for patient movement or movement of medical imaging device 116, is performed prior to procedure 1016.
15 Normalization is discussed in procedure 702 with reference to Figure 7. Normalization may be performed immediately prior to procedure 1014 or immediately after procedure 1014. The correlation procedure transforms the three-dimensional position magnetic coordinate into a three-dimensional coordinate in the optical coordinate system. The correlation
20 procedure is based on the magnetic-optical transformation model, determined in procedure 210 with reference to Figure 2.

In procedure 1018, optical projection is performed on each correlated cardiac trajectory shifted in procedure 1014. The optical projection procedure transforms the three-dimensional position MPS
25 coordinate in the optical coordinate system to a two-dimensional optical coordinate. The optical projection procedure is based on the three-dimensional to two-dimensional optical transformation model, determined in procedure 228 with reference to Figure 2. It is recalled that the three-dimensional to two-dimensional optical transformation model is time-
30 tagged. Therefore the optical projection procedure is based on a three-

dimensional to two-dimensional optical transformation which has the same time-tag as the cardiac trajectory.

In procedure 1020, each shifted centerline trajectory is superimposed onto the corresponding two-dimensional image. For each
5 two-dimensional image, the MPS coordinate readings of the centerline trajectory matching the same phase at the two-dimensional image are superimposed onto that image. The coordinate readings are then connected together by lines, thereby composing a spline representing the trajectory of surgical tool 124 respective of an activity state of the
10 inspected organ. Display 110 may present an image frame showing the position of surgical tool 124 respective of the inspected organ, at a given point in time, in accordance with acquired two-dimensional image data and acquired MPS data. Further, display 110 may present a motion picture showing the trajectory of the guided surgical tool respective of the
15 inspected organ, in accordance with acquired two-dimensional image data set and acquired MPS data set. The MPS data and two-dimensional image data may further be associated with activity state information. Display 110 may further simultaneously present a superimposition of current real-time MPS data on current real-time images, while presenting a superimposition
20 of the same current real-time MPS data on previously taken images, using associated activity state information.

It will be appreciated by persons skilled in the art that the disclosed technique is not limited to what has been particularly shown and described hereinabove. Rather the scope of the disclosed technique is
25 defined only by the claims, which follow.

CLAIMS

1. An apparatus for generating an organ timing signal relating to at least one inspected organ within the body of a patient, said apparatus comprising:

5 a medical positioning system (MPS) including:
 at least one reference electromagnetic transducer placed at
 a reference location;
 at least one inner electromagnetic transducer attached to a
 surgical tool inserted in a blood vessel in the vicinity of said
10 inspected organ; and
 an MPS processor, coupled with said at least one reference
 electromagnetic transducer and with said at least one inner
 electromagnetic transducer, said MPS processor determining
 the three-dimensional position of said at least one inner
15 electromagnetic transducer, by processing transmitted
 electromagnetic signals transmitted from at least one of said at
 least one reference electromagnetic transducer and said at least
 one inner electromagnetic transducer with detected
 electromagnetic signals detected by at least the other of said at
20 least one reference electromagnetic transducer and said at least
 one inner electromagnetic transducer, said MPS processor
 further generating MPS data sets, each of said MPS data sets
 comprising a collection of three-dimensional position coordinate
 readings demonstrating the motion trajectory of said surgical tool
25 over time; and
 a processor coupled with said MPS, generating said organ
 timing signal from said MPS data sets by detecting and identifying
 periodic motion frequencies in said MPS data sets, and filtering said
 periodic motion frequencies from said MPS data sets.

30

2. An apparatus for generating an organ timing signal relating to at least one inspected organ within the body of a patient, said apparatus being coupled with a medical positioning system (MPS), said medical positioning system transmitting and detecting electromagnetic signals between a reference location and a surgical tool inserted in the vicinity of said inspected organ, said medical positioning system determining a three-dimensional position of said surgical tool by processing said transmitted electromagnetic signals with said detected electromagnetic signals, said medical positioning system further generating MPS data sets, each of said MPS data sets comprising a collection of three-dimensional position coordinate readings demonstrating the motion trajectory of said surgical tool over time, said apparatus comprising:
- 5
- 10
- 15 a processor, generating said organ timing signal from said MPS data sets by detecting and identifying periodic motion frequencies in said MPS data sets, and by filtering said periodic motion frequencies from said MPS data sets.
- 20 3. The apparatus according to Claim 1, wherein said reference electromagnetic transducer transmits electromagnetic signals and said inner electromagnetic transducer detects electromagnetic signals.
- 25 4. The apparatus according to Claim 1, wherein said inner electromagnetic transducer transmits electromagnetic signals and said reference electromagnetic transducer detects electromagnetic signals.
- 30 5. The apparatus according to Claim 1, wherein for at least one of said at least one reference electromagnetic transducer, said reference location is a portion of said body of a patient.

6. The apparatus according to Claim 1, wherein for at least one of said at least one reference electromagnetic transducer, said reference location is stationary with respect to said body of a patient.
- 5
7. The apparatus according to Claim 1, further comprising at least one additional electromagnetic transducer attached to an area of said body of a patient, said electromagnetic transducer obtaining three-dimensional position information of said area, for movement
- 10 compensation.
8. The apparatus according to Claim 1, further comprising at least one additional electromagnetic transducer attached to a known area on the surface on which said patient rests, said electromagnetic
- 15 transducer obtaining three-dimensional position information of said area, for compensating for movement of said patient.
9. The apparatus according to Claim 1, wherein said processor further reconstructs a cardiac trajectory from said MPS data sets and said
- 20 filtered periodic motion frequencies, said cardiac trajectory representing the mechanical movement of said blood vessel originating from cardiac motion.
10. The apparatus according to Claim 1, wherein said processor further reconstructs a respiratory trajectory from said MPS data sets and
- 25 said filtered periodic motion frequencies, said respiratory trajectory representing the mechanical movement of said blood vessel originating from respiratory motion.

11. The apparatus according to Claim 9, wherein said processor further detects phase information of said inspected organ by identifying a plurality of phases on said reconstructed cardiac trajectory.
- 5 12. The apparatus according to Claim 10, wherein said processor further detects phase information of said inspected organ by identifying a plurality of phases on said reconstructed respiratory trajectory.
13. The apparatus according to Claim 1, wherein said inspected organ is
10 a heart.
14. The apparatus according to Claim 1, wherein said inspected organ is a lung.
- 15 15. The apparatus according to Claim 1, further comprising a database coupled with said MPS and with said processor, said database storing at least said MPS data sets.
16. The apparatus according to Claim 15, further comprising a medical
20 imaging device coupled with said database, said medical imaging device including an image detector, said medical imaging device acquiring a plurality of two-dimensional images of said inspected organ via said image detector, said database further storing at least said plurality of two-dimensional images.
- 25 17. The apparatus according to Claim 16, wherein one of said at least one reference electromagnetic transducer is attached to said image detector, obtaining external optical parameters relating to said medical imaging device.

30

18. The apparatus according to Claim 1, wherein one of said at least one inner electromagnetic transducer is coupled with an image sensor.
19. The apparatus according to Claim 1, further comprising an additional
5 electromagnetic transducer coupled with an image sensor.
20. The apparatus according to Claim 1, wherein said reference location is associated with an image sensor.
- 10 21. The apparatus according to Claim 11, further comprising:
a database coupled with said MPS and with said processor, said database storing at least said MPS data sets; and
a medical imaging device coupled with said database, said medical imaging device including an image detector, said medical
15 imaging device acquiring a plurality of two-dimensional images of said inspected organ via said image detector, said database further storing at least said plurality of two-dimensional images,
wherein said processor further associates between said acquired two-dimensional images, said MPS data sets, and said
20 phase information, and constructs trajectories of said surgical tool guided within said blood vessel, respective of different phases of said inspected organ.
22. The apparatus according to Claim 16, wherein said medical imaging
25 device includes an image acquisition system selected from the list consisting of:
ultrasound;
intra-vascular ultrasound;
X-ray;
30 C-arm machine;
fluoroscopy;

angiography;
computerized tomography;
nuclear magnetic resonance;
positron-emission tomography; and
5 single-photon-emission tomography.

23. The apparatus according to Claim 16, further comprising a display
coupled with said processor, said display presenting a motion picture
of said inspected organ, said motion picture presenting the trajectory
10 of said surgical tool guided within said blood vessel, respective of
different phases of said inspected organ.

24. The apparatus according to Claim 23, wherein said display presents a
single image frame in said motion picture, respective of the real-time
15 activity-state of said inspected organ.

25. The apparatus according to Claim 23, wherein said display presents a
playback of previous images in said motion picture, showing progress
of said surgical tool during previous activity-states of said inspected
20 organ.

26. The apparatus according to Claim 23, wherein said display is selected
from the list consisting of:
a two-dimensional display;
25 an auto-stereoscopic display viewed with a suitable pair of
spectacles;
a stand alone stereoscopic display; and
a pair of goggles.

30 27. The apparatus according to Claim 23, wherein said display includes
multiple monitors.

28. The apparatus according to Claim 27, wherein one of said monitors presents current *real-time* three-dimensional position data of said surgical tool superimposed on the current image frame of said inspected organ respective of the current activity-state, while another
5 of said monitors presents the current real-time three-dimensional position data of said surgical tool superimposed on a previous image frame of said inspected organ respective of a previous activity-state.
- 10 29. The apparatus according to Claim 23, wherein said display includes separate windows within a single monitor.
30. The apparatus according to Claim 29, wherein one of said windows presents current real-time three-dimensional position data of said surgical tool superimposed on the current image frame of said
15 inspected organ respective of the current activity-state, while another of said windows presents the current real-time three-dimensional position data of said surgical tool superimposed on a previous image frame of said inspected organ respective of a previous activity-state.
- 20 31. The apparatus according to Claim 21, wherein said processor associates between said plurality of two-dimensional images and said MPS data sets, with respect to said phase information at the time of acquisition or measurement.
- 25 32. The apparatus according to Claim 21, wherein said processor associates for a given two-dimensional image acquired during a given phase of said inspected organ, position coordinate readings detected during said given phase.
- 30

33. The apparatus according to Claim 21, wherein said processor constructs trajectories of said surgical tool guided within said blood vessel, based on said position coordinate readings detected during a given phase of said inspected organ.

5

34. The apparatus according to Claim 33, wherein said processor further associates each of said constructed trajectories with a two-dimensional image acquired during the corresponding phase of said inspected organ.

10

35. The apparatus according to Claim 33, wherein said display presents a superimposition of said constructed trajectories on its respective two-dimensional image.

15 36. The apparatus according to Claim 35, wherein said display presents said images as a series of individual image frames that are shown one at a time.

20 37. The apparatus according to Claim 35, wherein said display presents said images as a sequence of image frames that are shown consecutively.

25 38. Method for generating an organ timing signal relating to an inspected organ within the body of a patient, the method comprising the procedures of:

transmitting electromagnetic signals and detecting said electromagnetic signals;

processing said transmitted electromagnetic signals with said detected electromagnetic signals;

30 determining the three-dimensional position of a surgical tool inserted within the body of a patient based on said processing;

generating MPS data sets comprising a collection of three-dimensional position coordinate readings demonstrating the motion trajectory of said surgical tool over time;

detecting and identifying periodic motion frequencies in said MPS data sets; and

filtering said periodic motion frequencies from said MPS data sets.

39. The method according to Claim 38, further comprising the procedures of:

reconstructing the cardiac trajectory from said MPS data sets and said filtered periodic motion frequencies, said cardiac trajectory representing the mechanical movement of said blood vessel originating from cardiac motion;

reconstructing the respiratory trajectory from said MPS data sets and said filtered periodic motion frequencies, said respiratory trajectory representing the mechanical movement of said blood vessel originating from respiratory motion;

detecting phases of said inspected organ by identifying a plurality of phases on either of said reconstructed cardiac trajectory or said reconstructed respiratory trajectory; and

associating said phases with said MPS data sets, thereby obtaining phase information relating to said inspected organ.

40. The method according to Claim 39, further comprising the procedure of:

acquiring a plurality of two-dimensional images of said inspected organ.

41. The method according to Claim 40, further comprising the procedure of:

associating between said plurality of two-dimensional images, said MPS data sets, and said phase information.

5

42. The method according to Claim 41, wherein said plurality of two-dimensional images are associated between said MPS data sets, with respect to said phase information at the time of acquisition or measurement.

10

43. The method according to Claim 41, wherein a given one of said plurality of two-dimensional images acquired during a given phase is associated with position coordinate readings detected during said given phase at any cycle of said cardiac trajectory.

15

44. The method according to Claim 40, further comprising the procedures of:

normalizing one of said MPS data sets;

performing magnetic-optical correlation on said normalized MPS data sets;

20

performing optical projection on said correlated MPS data set, said correlated MPS data set comprising three-dimensional coordinate readings in the optical domain; and

superimposing said projected MPS data set onto a two-dimensional image selected from said acquired plurality of two-dimensional images, said projected MPS data set comprising two-dimensional coordinate readings in the optical domain,

25

thereby superimposing MPS data onto two-dimensional image data for corresponding data sets.

30

45. The method according to Claim 40, further comprising the procedures of:

obtaining phase information relating to said inspected organ from said MPS data sets for a first MPS data set selected from said MPS data sets, said first MPS data set being corresponding with a two-dimensional images data set;

obtaining phase information relating to said inspected organ from said MPS data sets for a second MPS data set selected from said MPS data sets, said second MPS data set being non-corresponding with said two-dimensional images data set; and

generating a third MPS data set from said second MPS data set using phase alignment between phases of said first MPS data set and said second MPS data set, said third MPS data set having the same time-tag as said first MPS data set.

46. The method according to Claim 45, further comprising the procedures of:

performing magnetic-optical correlation on said third MPS data set, said third MPS data set comprising three-dimensional coordinate readings in the magnetic domain;

performing optical projection on said correlated third MPS data set, said correlated third MPS data set comprising three-dimensional coordinate readings in the optical domain; and

superimposing said projected third MPS data set onto a two-dimensional image selected from said acquired plurality of two-dimensional images, said projected third MPS data set comprising two-dimensional coordinate readings in the optical domain,

thereby superimposing MPS data onto two-dimensional image data for non-corresponding data sets.

47. The method according to Claim 45, wherein said phase information is cardiac phase information.
48. The method according to Claim 45, wherein said phase information is
5 respiratory phase information.
49. The method according to Claim 45, wherein said phase information is cardiac phase information and respiratory phase information.
- 10 50. The method according to Claim 40, further comprising the procedures of:
obtaining phase information relating to said inspected organ from said MPS data sets for a selected one of said MPS data sets;
obtaining correlated phase information for a two-dimensional
15 images data set selected from said acquired plurality of two-dimensional images; and
generating a separate MPS data set for each two-dimensional image in said two-dimensional images data set, in accordance with image phase and time-tags.
- 20 51. The method according to Claim 50, further comprising the procedures of:
performing magnetic-optical correlation on each of said generated MPS data sets, each of said generated MPS data sets
25 comprising three-dimensional coordinate readings in the magnetic domain;
performing optical projection on each of said correlated MPS data sets, each of said correlated MPS data sets comprising three-dimensional coordinate readings in the optical domain; and
30 superimposing each of said projected MPS data sets onto corresponding two-dimensional image selected from said two-

dimensional images data set, said projected third MPS data set comprising two-dimensional coordinate readings in the optical domain,

5 thereby constructing trajectories of said surgical tool guided within a blood vessel in the vicinity of said inspected organ within the body of a patient, respective of different phases of said inspected organ.

52. The method according to Claim 50, wherein said phase information is
10 cardiac phase information.

53. The method according to Claim 50, wherein said phase information is respiratory phase information.

15 54. The method according to Claim 50, wherein said phase information is cardiac phase information and respiratory phase information.

55. The method according to Claim 51, wherein said constructed trajectories are presented on a display.
20

56. The method according to Claim 40, further comprising the procedures of:

obtaining phase information relating to said inspected organ from said MPS data sets for a selected one of said MPS data sets;

25 reconstructing the centerline trajectory from said MPS data sets and said filtered periodic motion frequencies, said centerline trajectory representing the central axis of the guiding motion of said surgical tool;

30 reconstructing separate centerline trajectories for each phase, in accordance with time-tags and detected phases of said reconstructed cardiac trajectory;

obtaining correlated phase information for a two-dimensional images data set selected from said acquired plurality of two-dimensional images; and

5 shifting each of said centerline trajectories by superimposing matching periodic motion components, for each phase of the two-dimensional images in said two-dimensional images data set.

57. The method according to Claim 56, further comprising the procedures of:

10 performing magnetic-optical correlation on each of said shifted centerline trajectories, each of said shifted centerline trajectories comprising three-dimensional coordinate readings in the magnetic domain;

15 performing optical projection on each of said shifted centerline trajectories, each of said shifted centerline trajectories comprising three-dimensional coordinate readings in the optical domain; and

20 superimposing each of said shifted centerline trajectories onto corresponding two-dimensional image selected from said two-dimensional images data set, each of said shifted centerline trajectories comprising two-dimensional coordinate readings in the optical domain,

25 thereby constructing trajectories of said surgical tool guided within a blood vessel in the vicinity of said inspected organ within the body of a patient, respective of different phases of said inspected organ.

58. The method according to Claim 56, wherein said phase information is cardiac phase information.

30 59. The method according to Claim 56, wherein said phase information is respiratory phase information.

60. The method according to Claim 56, wherein said phase information is cardiac phase information and respiratory phase information.
- 5 61. The method according to Claim 57, wherein said constructed trajectories are presented on a display.
62. The method according to Claim 38, wherein said inspected organ is a heart.
- 10 63. The method according to Claim 38, wherein said inspected organ is a lung.
- 15 64. The apparatus according to any of the claims 1-37 substantially as described herein above or as illustrated in any of the drawings.
65. The method according to any of the claims 38-63 substantially as described herein above or as illustrated in any of the drawings.

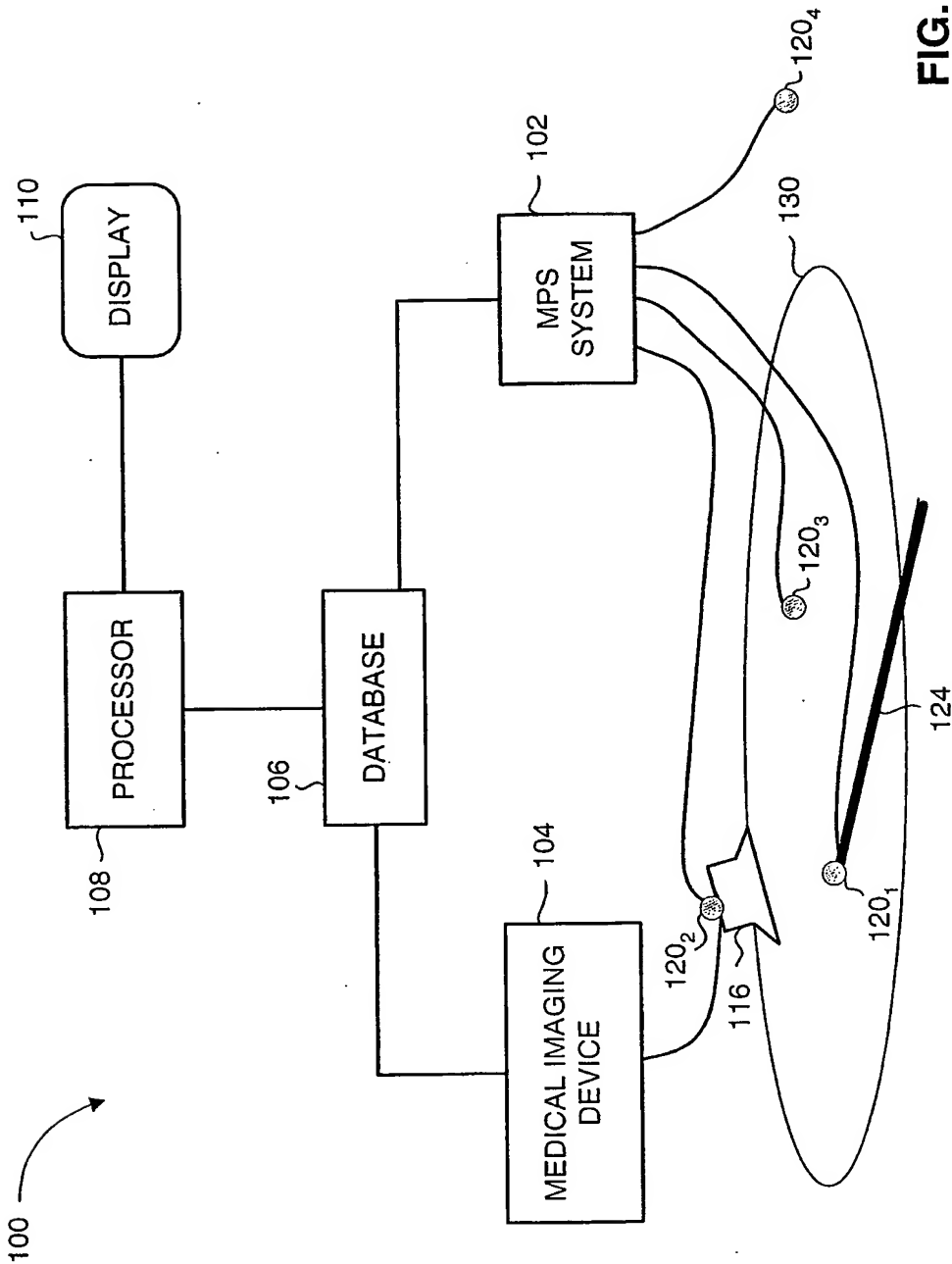


FIG. 1

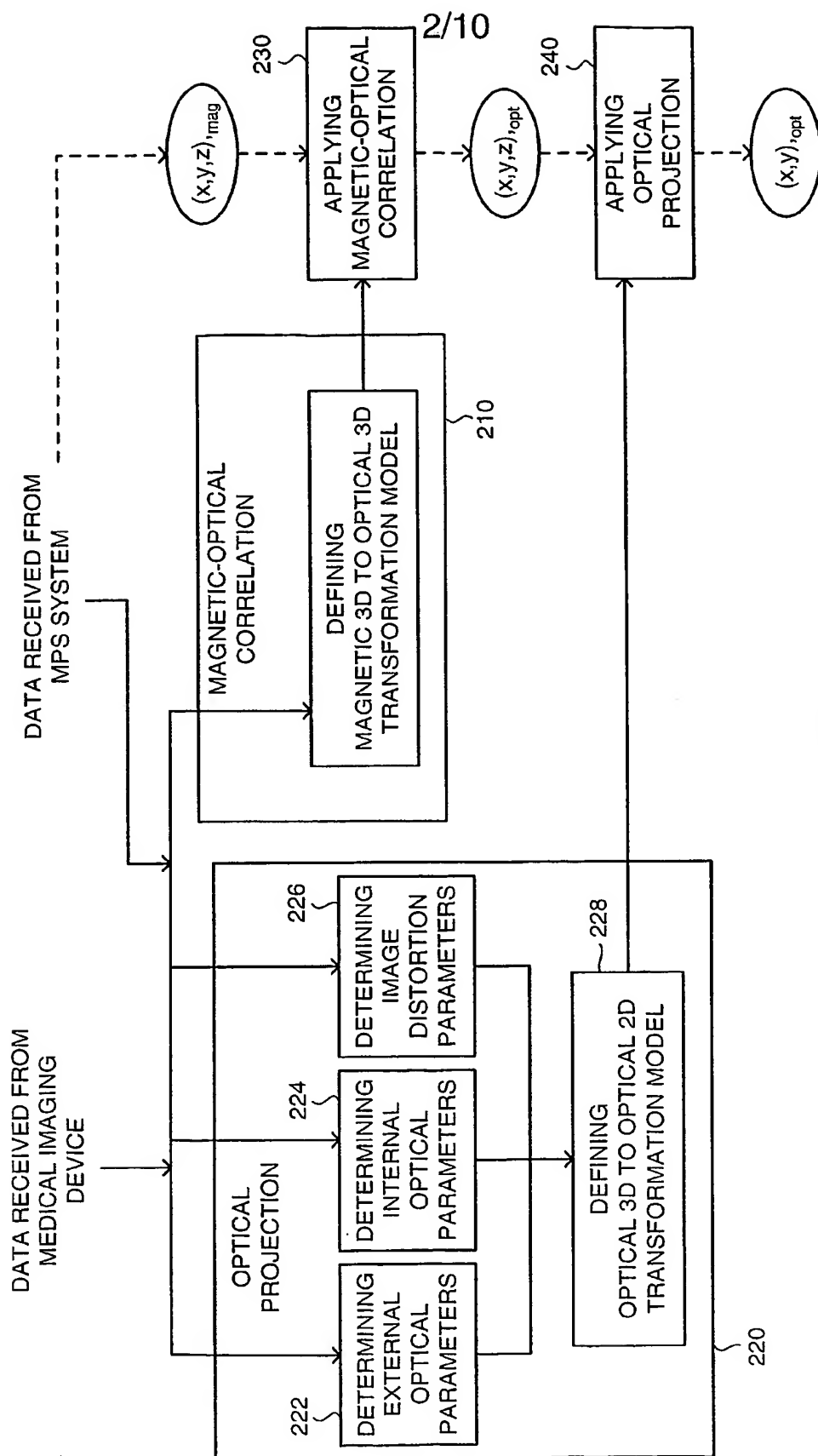


FIG. 2

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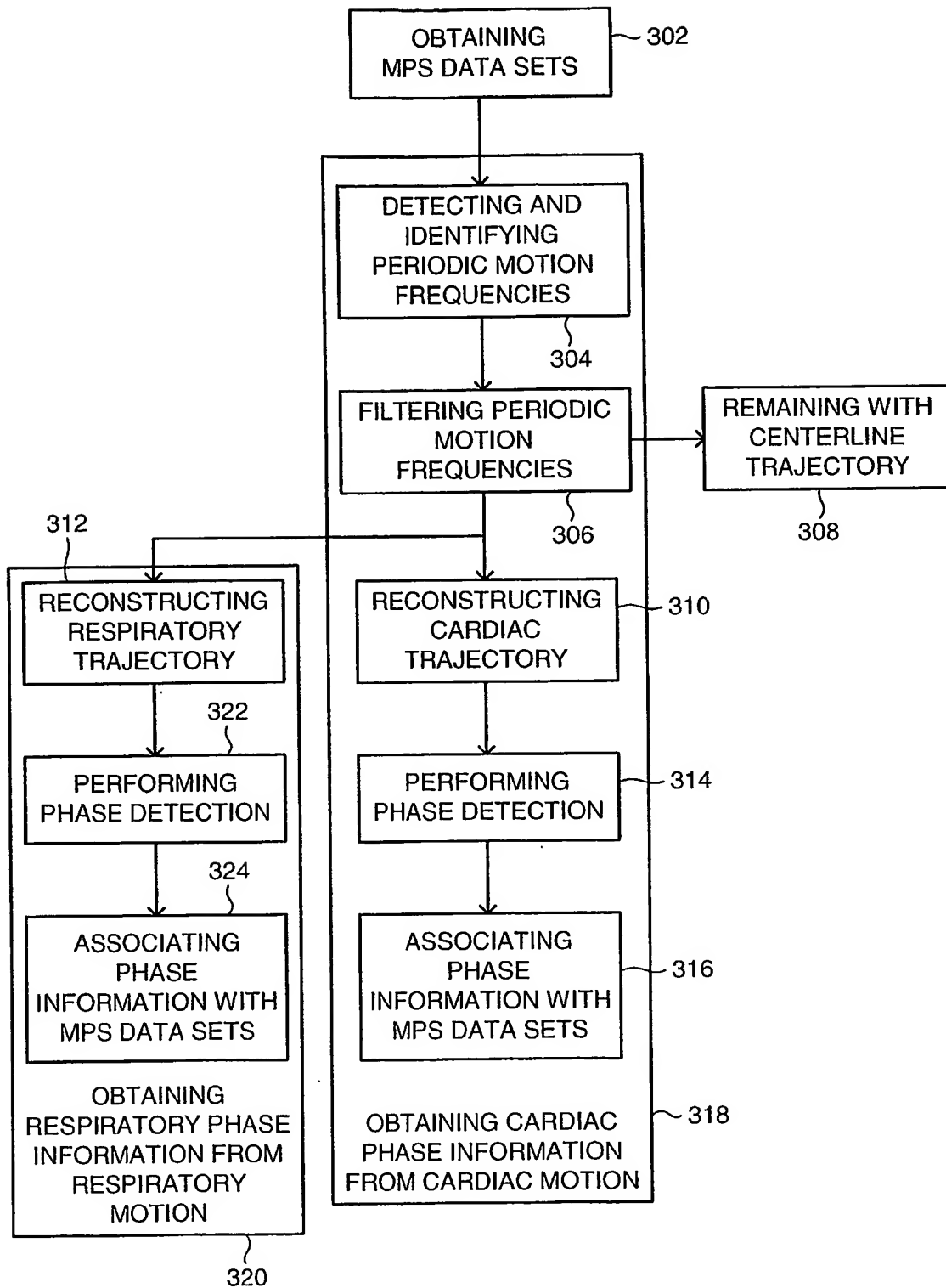
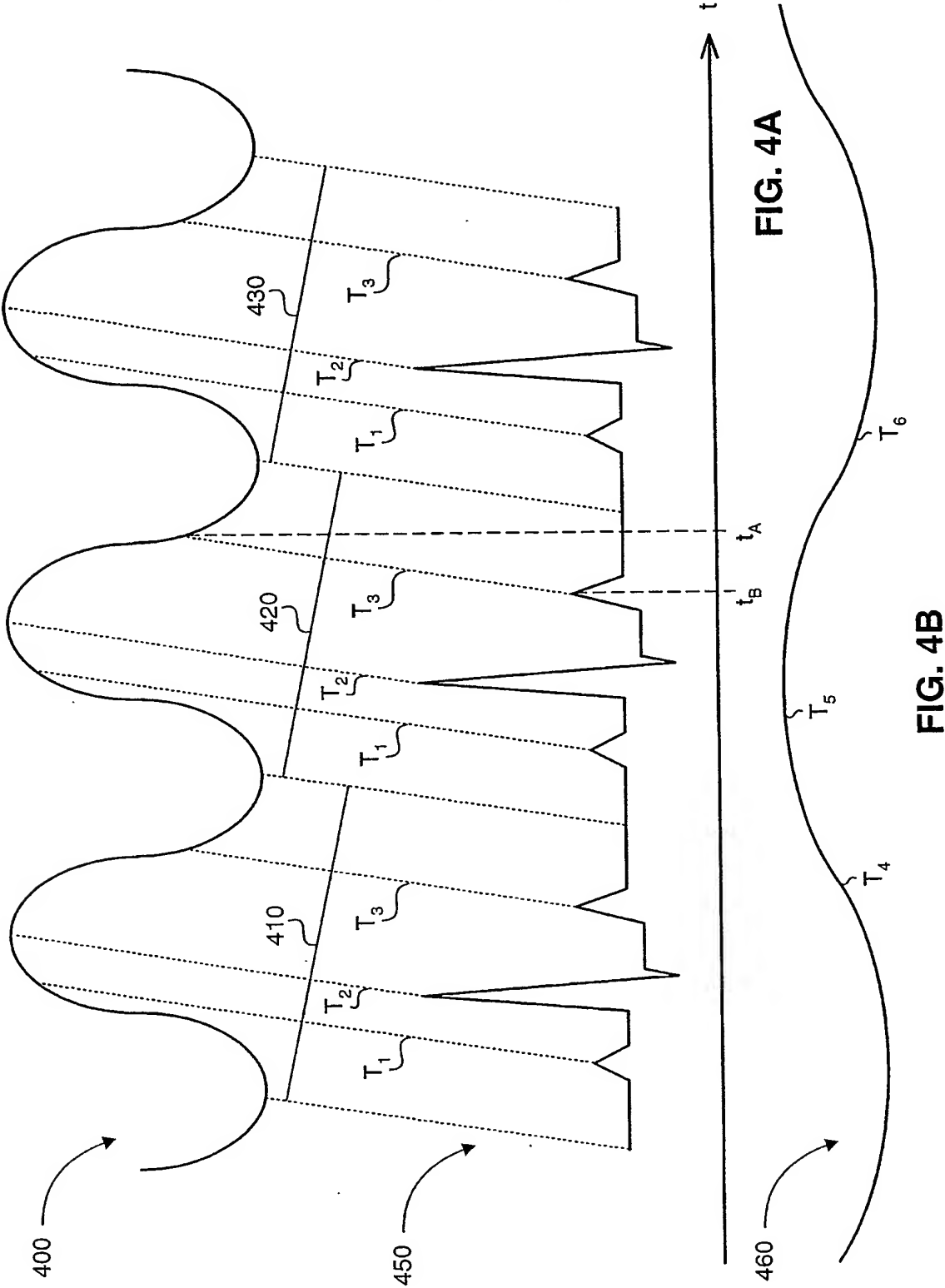


FIG. 3



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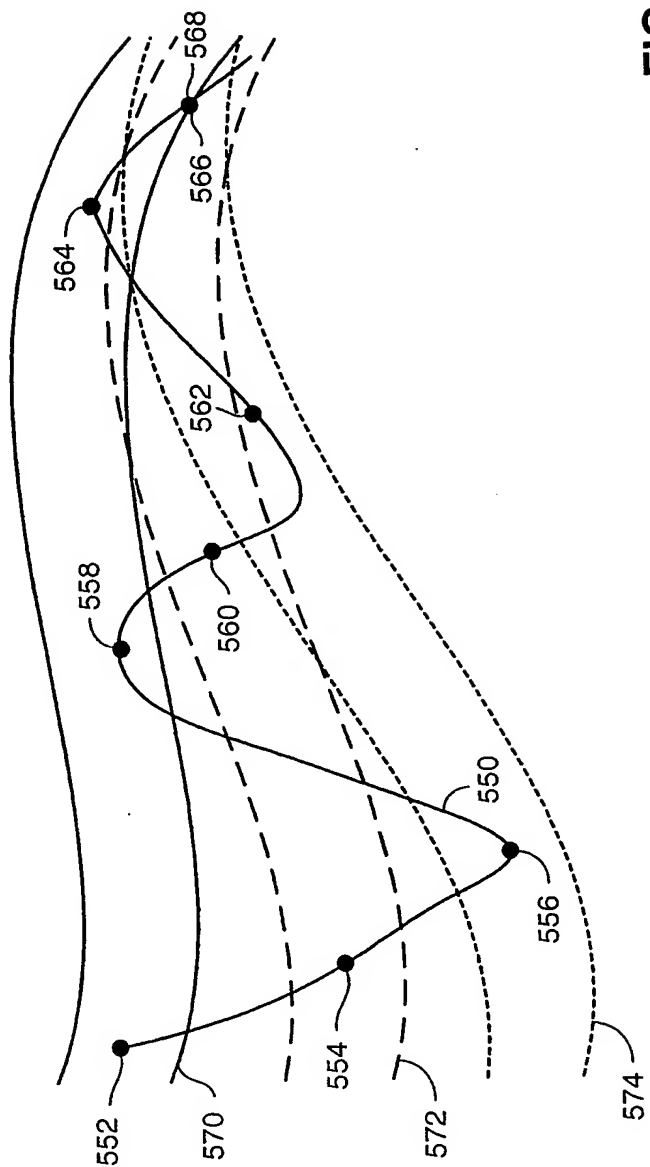


FIG. 5

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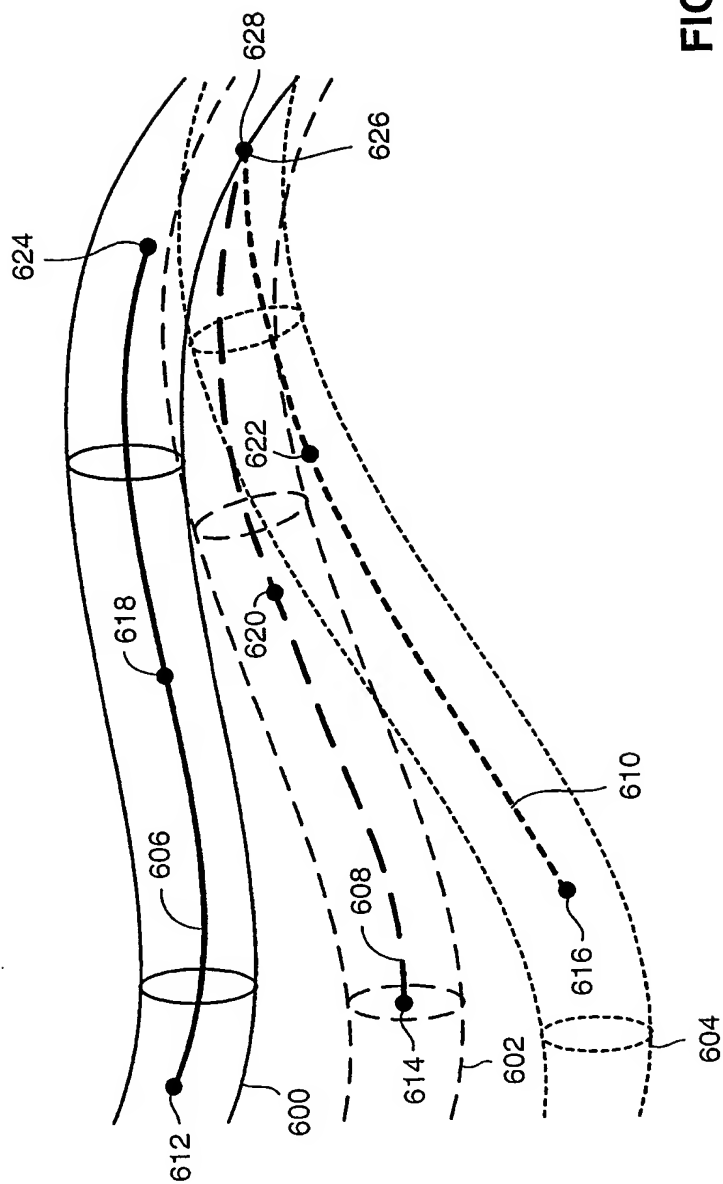


FIG. 6

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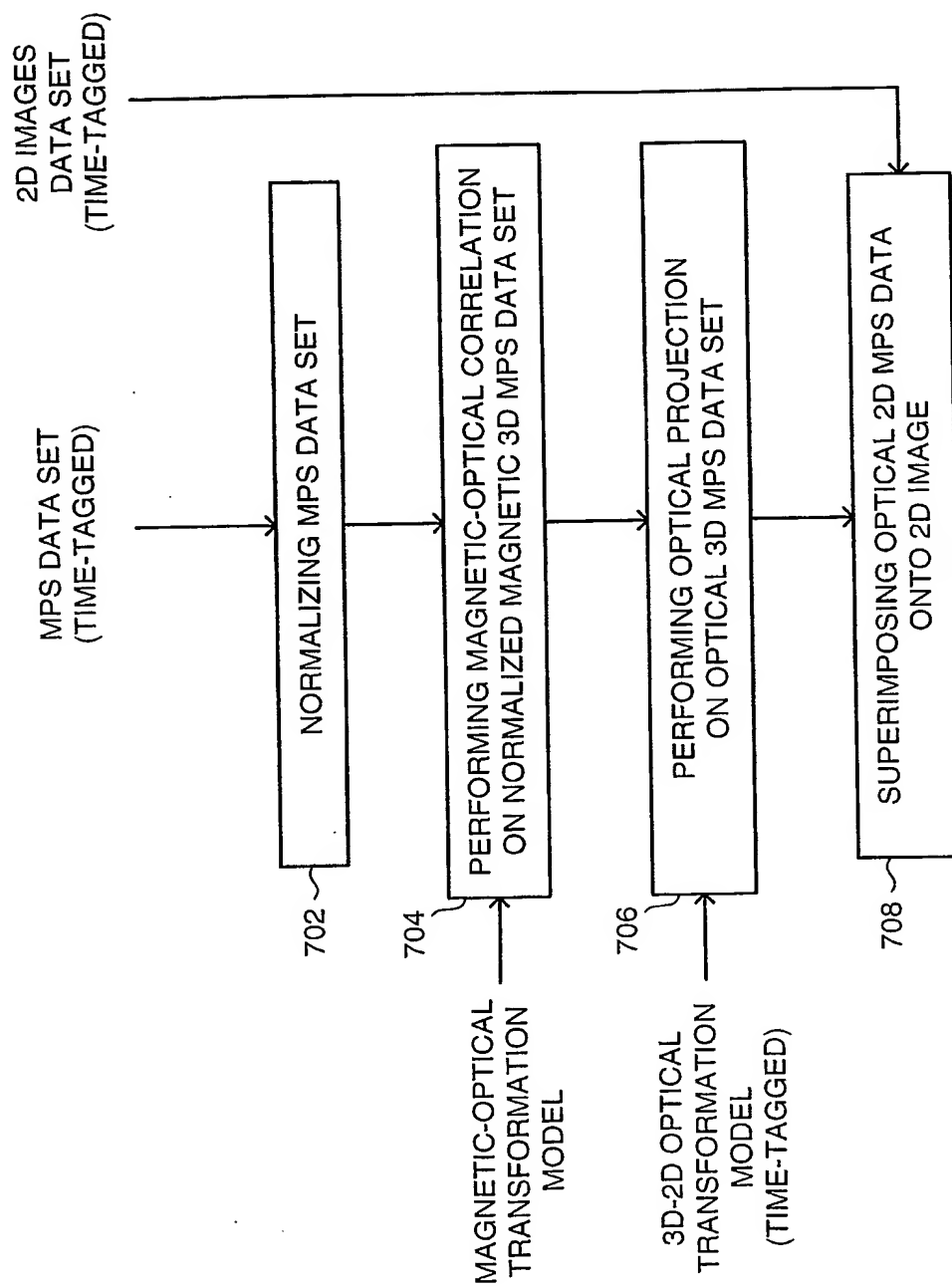


FIG. 7

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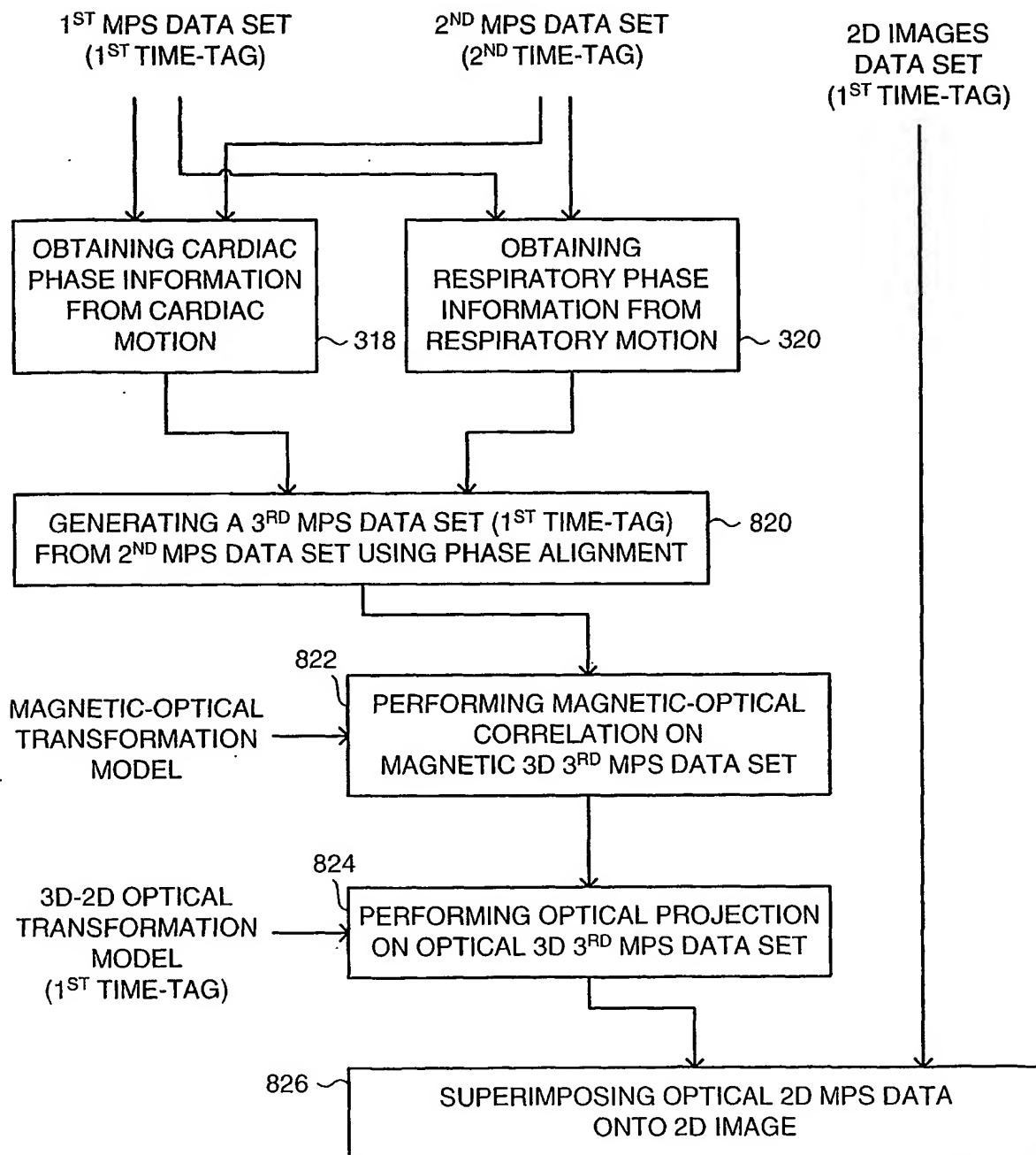


FIG. 8

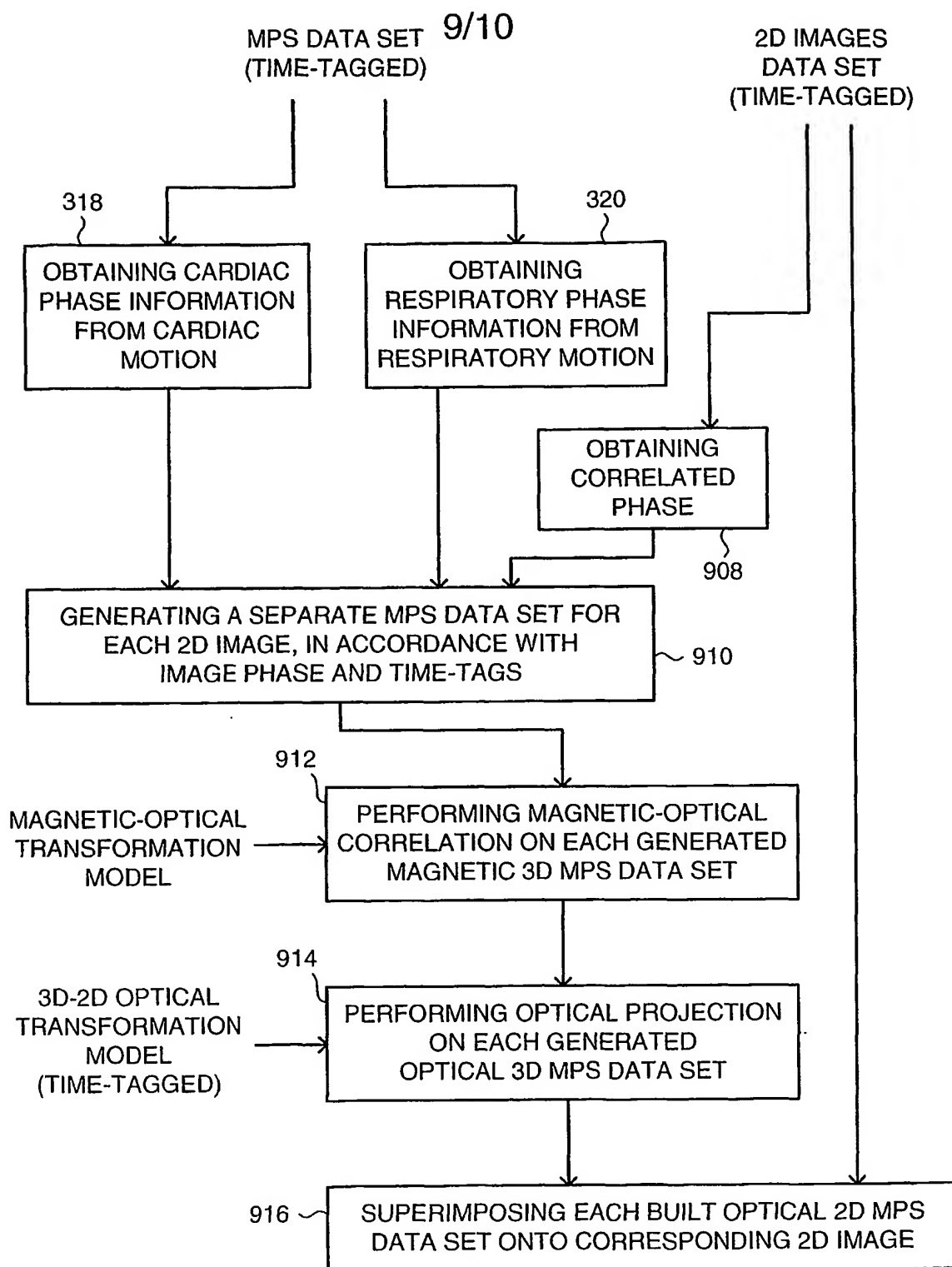


FIG. 9

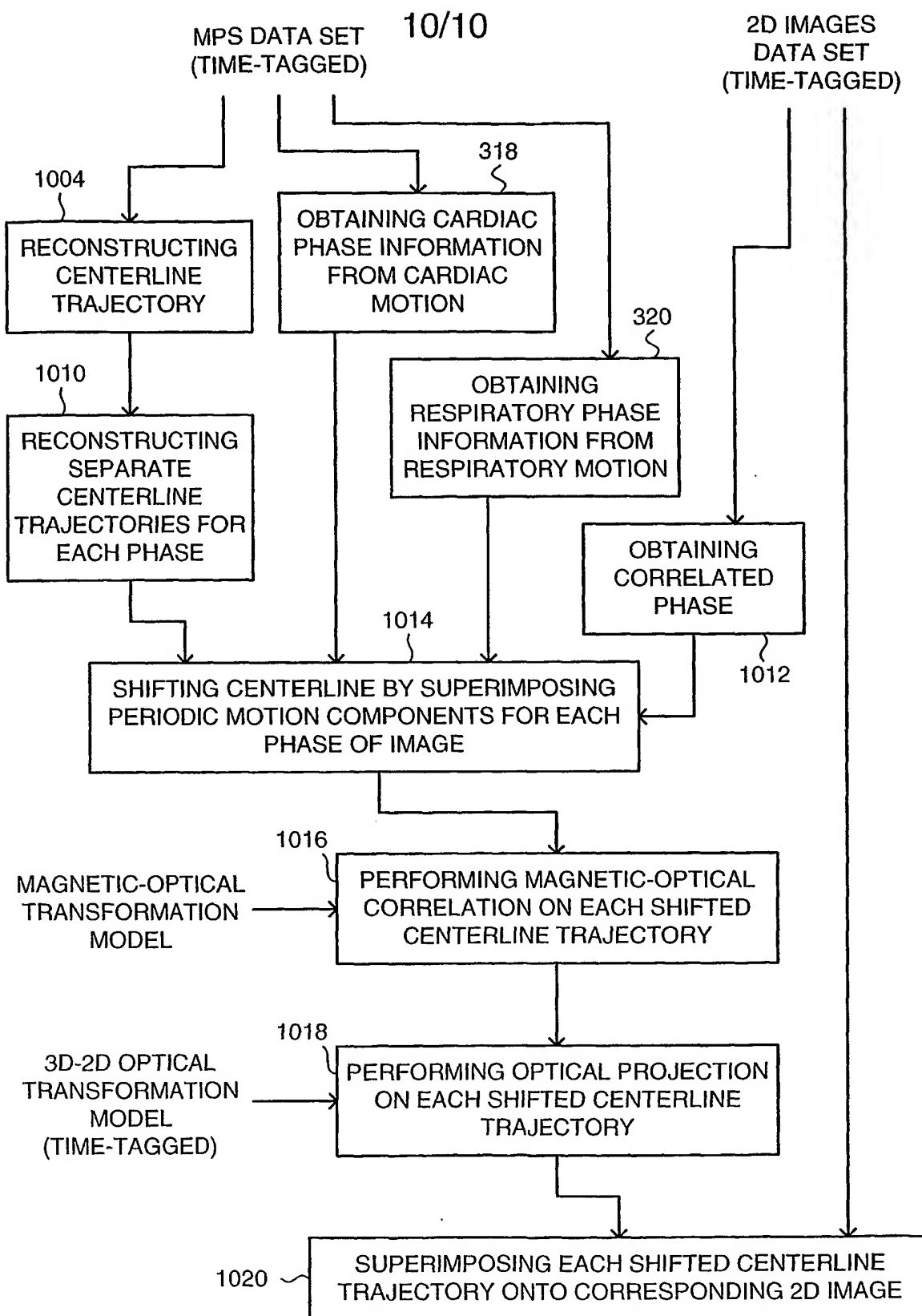


FIG. 10